

PATENT APPLICATION

NASA Case No. GSC13,817-4

EMPIRICAL MODE DECOMPOSITION FOR ANALYZING ACOUSTICAL SIGNALS

CROSS-REFERENCES TO RELATED APPLICATIONS

This Application is a Continuation-In-Part of Application No. 10/011,206, "Empirical Mode Decomposition Apparatus, Method and Article of Manufacture for Analyzing Biological Signal and Performing Curve Fitting, filed on December 10, 2001, which itself claims priority under U.S.C. §120 to parent application Serial No. 09/282,424 filed on March 31, 1999, which itself claims priority under U.S.C. §120 to parent application Serial No. 08/872,586 filed on June 10, 1997, which itself claims priority under 35 U.S.C. §119(e) to U.S. Provisional application Serial No. 60/023,411 filed on August 14, 1996 and Serial No. 60/023,822 filed on August 12, 1996. This application claims priority under 35 U.S.C. §119(e) to U.S. Provisional application Serial No. 60/266,422 filed on February 14, 2001. All of the above provisional and non-provisional patent applications are hereby incorporated by reference.

ORIGIN OF INVENTION

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BACKGROUND OF THE INVENTION

This invention generally relates to a signal analysis method. The results of processing several examples of
15 biological and acoustical signals are discussed herein to show the particular utility of the invention in that field and to further demonstrate the broad applicability of the invention.

Although the present invention finds utility in processing acoustical signals, it is to be understood that any
20 signal representative of a real world phenomenon such as a signal representative of a physical process including electrical, mechanical, biological, acoustical, chemical, optical, geophysical or other process(es) may be analyzed and thereby more fully understood by applying the invention
25 thereto. The real world signals to which the invention finds utility include a wide variety of real world phenomena such as the behavior of a stock market, population growth, traffic flow, etc.. Furthermore, the term "real world signal" also includes "physical signals" representative of physical
30 processes such as the electrical, mechanical, biological, chemical, acoustical, optical, geophysical process(es) mentioned above.

Although the invention is not limited to a particular type of signal processing and includes the full range of real

world data representative of processes or phenomena or combinations thereof, it is most useful when such real world signals are nonlinear and nonstationary.

DESCRIPTION OF RELATED ART

In the parent application, several examples of geophysical data signals representative of earthquakes, ocean waves, tsunamis, ocean surface elevation and wind were processed to show the invention's wide utility to a broad variety of signal types. The techniques disclosed therein and elaborated upon herein represent major advances in physical signal processing.

Previously, analyzing signals, particularly those having nonlinear and/or nonstationary properties, was a difficult problem confronting many industries. These industries have harnessed various computer implemented methods to process data signals measured or otherwise taken from various processes such as electrical, mechanical, optical, biological, and chemical processes. Unfortunately, previous methods have not yielded results which are physically meaningful.

Among the difficulties found in conventional systems is that representing physical processes with physical signals may present one or more of the following problems:

- (a) The total data span is too short;
- (b) The data are nonstationary; and
- (c) The data represent nonlinear processes.

Although problems (a)-(c) are separate issues, the first two problems are related because a data section shorter than the longest time scale of a stationary process can appear to be nonstationary. Because many physical events are transient, the data representative of those events are nonstationary. For example, a transient event such as an earthquake will produce nonstationary data when measured. Nevertheless, the nonstationary character of such data is ignored or the effects

assumed to be negligible. This assumption may lead to inaccurate results and incorrect interpretation of the underlying physics as explained below.

A variety of techniques have been applied to nonlinear, nonstationary physical signals. For example, many computer implemented methods apply Fourier spectral analysis to examine the energy-frequency distribution of such signals.

Although the Fourier transform that is applied by these computer implemented methods is valid under extremely general conditions, there are some crucial restrictions: the system must be linear, and the data must be strictly periodic or stationary. If these conditions are not met, then the resulting spectrum will not make sense physically.

A common technique for meeting the linearity condition is to approximate the physical phenomena with at least one linear system. Although linear approximation is an adequate solution for some applications, many physical phenomena are highly nonlinear and do not admit a reasonably accurate linear approximation.

Furthermore, imperfect probes/sensors and numerical schemes may contaminate data representative of the phenomenon. For example, the interactions of imperfect probes with a perfect linear system can make the final data nonlinear.

Many recorded physical signals are of finite duration, nonstationary, and nonlinear because they are derived from physical processes that are nonlinear either intrinsically or through interactions with imperfect probes or numerical schemes. Under these conditions, computer implemented methods which apply Fourier spectral analysis are of limited use. For lack of alternatives, however, such methods still apply Fourier spectral analysis to process such data.

In summary, the indiscriminate use of Fourier spectral analysis in these methods and the adoption of the stationarity

and linearity assumptions may give inaccurate results some of which are described below.

First, the Fourier spectrum defines uniform harmonic components globally. Therefore, the Fourier spectrum needs many additional harmonic components to simulate nonstationary data that are nonuniform globally. As a result, energy is spread over a wide frequency range.

For example, using a delta function to represent the flash of light from a lightning bolt will give a phase-locked wide white Fourier spectrum. Here, many Fourier components are added to simulate the nonstationary nature of the data in the time domain, but their existence diverts energy to a much wider frequency domain. Constrained by the conservation of energy principle, these spurious harmonics and the wide frequency spectrum cannot faithfully represent the true energy density of the lighting in the frequency and time space.

More seriously, the Fourier representation also requires the existence of negative light intensity so that the components can cancel out one another to give the final delta function representing the lightning. Thus, the Fourier components might make mathematical sense, but they often do not make physical sense when applied.

Although no physical process can be represented exactly by a delta function, some physical data such as the near field strong earthquake energy signals are of extremely short duration. Such earthquake energy signals almost approach a delta function, and they always give artificially wide Fourier spectra.

Second, Fourier spectral analysis uses a linear superposition of trigonometric functions to represent the data. Therefore, additional harmonic components are required to simulate deformed wave profiles. Such deformations, as will be shown later, are the direct consequence of nonlinear effects. Whenever the form of the data deviates from a pure

sine or cosine function, the Fourier spectrum will contain harmonics. Furthermore, both nonstationarity and nonlinearity can induce spurious harmonic components that cause unwanted energy spreading and artificial frequency smearing in the Fourier spectrum. In other words, the nonstationary, stochastic nature of biological data suffers from conventional signal processing techniques and makes the interpretation of the processed data quite difficult.

Biological Signal Analysis

According to the above background, there is a need for a more accurate signal processing technique that produces results that are more physically meaningful and readily understood. Biological signals provide another example of physical signals in which this invention is applicable. Parent application serial no. 08/872,586 filed June 10, 1997 and now issued, U.S. Patent No. 5,983,162, illustrates several other types of signals in which this invention is applicable. Namely, the patent provides specific examples of nonlinear, nonstationary geophysical signals which are very difficult to analyze with traditional computer implemented techniques including earthquake signals, water wave signals, tsunami signals, ocean altitude and ocean circulation signals.

Many of the aforementioned signal processing problems exist when biological signals are processed. For example, most data in the field of biology are nonstationarily stochastic. When conventional tools such as Fourier Analysis are applied to such biological data, the result often-times obscures the underlying processes. In other words, conventional Fourier analysis of biological data throws away or otherwise obscures valuable information. Thus, the complex biological phenomena producing such data cannot be readily understood and is, in any event, represented imprecisely. The interpretation of the results of such conventionally processed

data may, therefore, be quite difficult. The conventional techniques also make accurate modelling of the biological phenomena very difficult and, sometimes, impossible.

5 Acoustical Signal Analysis

The idea of recording and transmitting sounds and speeches depends, for example, on the variations of the density in the air, and currents in the telephone. The crucial element is on the **variation**, without which the sound would be a monotonic tone that would not carry any information. Speech consists of time varying acoustical signals, which are nonstationary and nonlinear. In fact, for the acoustical signal to carry any information at all, be it speech or music notes, there must be a time variation in amplitude and frequency continuously and, may be, subtly. Unfortunately, the tools we have to deal with nonstationary processes are quite limited; therefore, we are forced to make all kinds of approximations: As a result, there is a conflict between the human perception and automatic sound processes.

Some publications listed, relating to acoustical signal analysis, are incorporated by reference:

Allen, J. B., 1994: How do humans process and recognize speech? IEEE Trans. Speech and Audio Proc., 2, 567-577.

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George, D. E. and E. Salari, 1997: Real-time pitch extraction of voiced speech, J. Network and Computer Applications, 20, 379-387.

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Li, T. H, and J. D. Gibson, 1996: Speech analysis and segmentation by parametric filtering, IEEE Trans. Speech and Audio Proc., 4, 203-213.

Loughlin, P. J., J. W. Pitton, and L. E. Atlas, 1994: Construction of positive time-frequency distributions, IEEE Trans. Signal Proc., 42, 2697-2705.

Loughlin, P. J., B. Tacer, 1996: On the amplitude- and frequency-modulation decomposition of signals, J. Acoust. Soc. Am., 100, 1594-1601.

Maragos, P., J. F. Kaiser, and T. F. Quatieri, 1993: Energy separation in signal modulations with application to speech analysis, IEEE Trans. Signal Processing, 41, 3024-3051.

Maragos, P. and A. Potamianos, 1999: Fractal dimensions of speech sounds: Computation and application to automatic speech recognition, J. Acoust. Soc. Am, 105, 1925-1932.

Picinbono, B., 1997: On the instantaneous amplitude and phase of signal, IEEE Trans. Signal Processing, 45, 552-560.

Pinter, Istvan, 1996: Perceptual wavelet-representation of speech signals and its application to speech enhancement. Computer Speech and language, 10, 1-22.

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Quatieri, T. F., T. E. Hanna, and G. C. O'Leary, 1997:
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speech recognition, IEEE Trans. Speech and Audio Proc.,
6, 36-48.

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Extraction of vocal-tract system characteristics from
speech signals. IEEE Trans. Speech and Audio Proc., 6,
313-327.

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An iterative algorithm for decomposition of speech
signals into periodic and aperiodic components, IEEE
Trans. Speech and Audio Proc., 6, 1-11.

Because our emphasis will be on speech analysis, we
should first examine the principles of Human Speech
35 Recognition (HSR) and Automatic (Machine) Speech Recognition
(ASR). As summarized in the classical paper by Allen (1994),
typical ASR systems start with a front end that transforms the
speech signal into a feature vector. This process is mostly
through spectral analysis over a fixed period of time, within
40 such period the speech signal is assumed to be **stationary**.
The analysis is strictly on frequency. HSR on the other hand,
processes information across frequency localized in time.
Thus, the process is assumed to be **nonstationary**. These
localized speech features are known as the formants. To
45 extract features localized in time but across all frequencies

requires time-frequency analysis. The speech signals are divided into a time-frequency continuum of formants by the cochlea of the ear, which, by its mechanical properties, is a very poor frequency discriminator. Yet, classic experiments by Shower and Biddulph (1931) has shown that the ear can detect frequency difference as small as 3 Hz near a signal of 1000 Hz. Such perceptual acuity for pitch seems to violate the 'uncertainty relation' for stationary processes, where $\Delta f \Delta t \geq \frac{1}{2}$, with Δf as the standard deviation of the frequency, and Δt as the given time period. Clearly, using the traditional method based on the stationary assumption cannot explain the HSR processes. Therefore, for an accurate sound perception, we need a different paradigm of sound signal analysis, one with time-frequency analysis. This is crucial for speech recognition. It is also the cause of the long standing difficulty in Speech recognition as stated in the classic book by Rabiner and Juang (1993): "Although there is a solid basis for the linguist description of sounds and a good understanding of the associates acoustics of sound production, there is, at best, a tenuous relationship between a given linguistic sound and a repeatable, reliable, measurable set of acoustic parameters." To overcome this difficulty, we need a new signal analysis method.

To deal with the nonstationary properties of speech, various methods have been employed (see, for example, the classical book by Rabiner and Schafer (1978), and more recent developments by Furui and Sonfhi (1992), Hoffman and Westendorf (1997)), that include spectral analysis, filter-bank, zero-crossing, pattern recognition dynamical programming, linear prediction, statistic methods, and neural network. In many of these approaches, there lies a tactic assumption that the speech can be treated as locally stationary. Although great progress has been made, in speech

recognition, the locally stationary assumption has rendered speech synthesis to bear a flat, wooden and artificial tone.

In addition to speech recognition, there are a wide variety of speech communications application that will depend on detailed signal analysis, such as digital transmission and storage of speech signals, speech synthesis, speaker verification and identification, and the enhancement of signal quality. The techniques used in all of these applications are not strictly limited to speeches alone, the same approach can also be applied to musical scores and recordings, and even to machine condition monitoring.

So far, we have only touched on the problem of nonstationary properties of the acoustical signal. A more important part is the nonlinear properties of the acoustical signal in general and speech in particular, which has mostly been neglected up until very recently (see, for example, Kumar, 1996). As it is well known that the sound in speech is generated by three mechanisms:

- (1) The vibration of the vocal chords,
- (2) The friction of air through constriction of the vocal tract, and
- (3) The explosion of a sudden release of the air from complete closure of the vocal tract.

Of the three mechanisms, the vowels are generated by the vibration of the vocal cord with unrestricted passage of air. Such sound can be generated for indefinite length as long as the lung can supply the airflow. Therefore, the vowels are the only sounds that could be approximated locally as stationary, but only locally. Unfortunately, in our speech, vowels are not the information carrying sounds, the consonants are. The consonant's varying of frequency is a necessity for

transmitting information. For example, if we write the sentence,

Do you understand what John just said.

as,

D- y- - -nd-rst-nd wh-t J-hn -jst s- -d.

Most people can still figure out the meaning of the utterance. On the other hand, if we would write the sentence as

-o - ou u- -e- - -a- - - - a- -o- - --- u- -ai-.

No one would be able to decipher what is its meaning at all. Consequently, in speech recognition, the precise analysis of the consonant signals is crucial.

Consonants are highly transient and the generating mechanisms are all nonlinear. Such nonlinearity has been known for a long time (See, for, example, Rabiner and Schafer, 1978), but only recently has there been any investigations (see, for example, Billa and El-Jaroudi, 1998; and Maragos and Potamianos, 1999). Although the locally stationary assumption can be used for vowels better than the consonants, we have to examine the consonants, for, as we have seen, consonants contain far more information than vowels. This creates obvious difficulties for the present approach in speech signal analysis using methods based on linear and stationary assumptions such as filter bank or spectrogram etc. Considering the generation mechanisms, we can immediately find that mechanisms involved in generating the consonants are all nonlinear. Therefore, we need a signal analysis method that

is not only applicable to nonstationary but also to nonlinear processes. The Empirical Mode Decomposition (EMD) is the only method known for the task. Previously, an application of the EMD as been the Hilbert-Huang Transform (HHT), as described in
5 previous patent applications and publications. In speech communication, we process information frequency and amplitude locally and instantaneously. The natural way is not to wait for a long string of data and then to process it spectrally. Built in with an intermittent test option, we can use EMD as a
10 perfect tool to construct a filter bank, but the filter is in temporal space rather than in frequency space. This temporal space filtering retains the full nonlinearity without resorting to the spurious harmonics. It also eliminates the distortion that could be introduced through Fourier based
15 frequency filtering. Therefore, EMD is a natural choice. The product of EMD is actually the formant components without the difficulties of frequency resolution in any range.

Speech signal analysis is the most fundamental requirement for speech synthesis, speaker verification and
20 identification, speech recognition, and enhancement and restoration of speech record. The basic technique can also be applied to processing music

SUMMARY OF THE INVENTION

25 An object of the present invention is to solve the above-mentioned problems in conventional signal analysis techniques.

Another object of the present invention is to provide further examples of physical signal processing thereby further demonstrating the broad applicability of the invention to a
30 wide array of physical signals which include acoustical signals.

Another object is to provide a technique of distilling a physical signal to the point at which the signal can be represented with an analytic function.

To achieve these objects, the invention employs a computer implemented Empirical Mode Decomposition method which decomposes physical signals representative of a physical phenomenon into components. These components are designated
5 as Intrinsic Mode Functions (IMFs) and are indicative of intrinsic oscillatory modes in the physical phenomenon.

Contrary to almost all the previous methods, this new computer implemented method is intuitive, direct, a *posteriori*, and adaptive, with the basis of the decomposition
10 based on and derived from the physical signal. The bases so derived have no close analytic expressions, and they can only be numerically approximated in a specially programmed computer by utilizing the inventive methods disclosed herein.

More specifically, the general method of the invention includes two main components or steps to analyze the physical
15 signal without suffering the problems associated with computer implemented Fourier analysis, namely inaccurate interpretation of the underlying physics or biology caused in part by energy spreading and frequency smearing in the Fourier spectrum.

The first step is to process the data with the Empirical Mode Decomposition (EMD) method, with which the data are decomposed into a number of Intrinsic Mode Function (IMF)
20 components. In this way, the signal will be expanded by using a basis that is adaptively derived from the signal itself.
25

The second step of the general method of the present invention is to apply the Hilbert Transform to the decomposed IMF's and construct an energy-frequency-time distribution, designated as the Hilbert Spectrum, from which occurrence of
30 physical events at corresponding times (time localities) will be preserved. There is also no close analytic form for the Hilbert Spectrum. As explained below, the invention avoids this problem by storing numerical approximations in the

specially programmed computer by utilizing the inventive method.

The invention also utilizes instantaneous frequency and energy to analyze the physical phenomenon rather than the global frequency and energy utilized by computer implemented Fourier spectral analysis.

Furthermore, a computer implementing the invention, e.g., via executing a program in software, to decompose physical signals into intrinsic mode functions with EMD and generate a Hilbert spectrum is also disclosed. Because of the lack of close form analytic expression of either the basis functions and the final Hilbert spectrum; computer implementation of the inventive methods is an important part of the overall method, however other implementation of the invention may be done.

Still further, the invention may take the form of an article of manufacture. More specifically, the article of manufacture is a computer-usable medium, including a computer-readable program code embodied therein wherein the computer-readable code causes a computer to execute the inventive method.

Once the IMF's are generated, the invention can then produce a distilled or otherwise filtered version of the original physical signal. This distillation process eliminates undesired IMF's and thereby generates a filtered signal from which it is possible to perform a curve fitting process. In this way, it is possible to arrive at an analytic function which accurately represents the physically important components of the original signal.

This invention discloses a method in which Hilbert spectrum generated from IMF decomposed from a first signal may be compared with another Hilbert Spectrum to determine identification of the first signal.

Further scope of applicability of the present invention will become apparent from the detailed description given

hereinafter. However, it should be understood that the detailed description and specific examples, while indicating preferred embodiments of the invention, are given by way of illustration only, since various changes and modifications within the spirit and scope of the invention will become apparent to those skilled in the art from this detailed description. Furthermore, all the mathematic expressions are used as a short hand to express the inventive ideas clearly and are not limitative of the claimed invention.

BRIEF DESCRIPTION OF DRAWINGS

The present invention will become more fully understood from the detailed description given hereinbelow and the accompanying drawings which are given by way of illustration only, and thus are not limitative of the present invention, and wherein:

Figure 1(a) is a high-level flowchart describing the overall inventive method which may be implemented on the computer system shown in Figure 2;

Figure 1(b) is a high-level flowchart describing the Sifting Process which may be implemented on the computer system shown in Figure 2;

Figure 1(c) is a continuation of the high-level flowchart in Figure 1(b) describing the Sifting Process which may be implemented on the computer system shown in Figure 2;

Figure 1(d) is a high-level flowchart describing EMD signal filtering and curve fitting which may be implemented on the computer system shown in Figure 2;

Figure 2 is a high-level block diagram of a computer system which may be programmed with the inventive with the result being a special purpose computer;

Figure 3(a) shows wind speed data in the form of a graph plotting wind speed as a function of time for explaining the

computer implemented Empirical Mode Decomposition method of the invention;

Figure 3(b) is a graph illustrating the upper envelope, lower envelope, envelope mean and original wind speed data which are utilized to explain the computer implemented Empirical Mode Decomposition method of the invention;

Figures 3(c)-(e) are graphs of the first, second and third component signals h_1 , h_{11} , h_{12} , respectively which are generated by the Sifting Process of the invention;

Figure 3(f) is a graph of the first intrinsic mode function component which is generated by the Sifting Process of the invention;

Figure 3(g) is a graph of data with intermittency for illustrating an optional intermittency test of the invention;

Figures 3(h)-(j) are graphs of the first, second, and third intrinsic mode functions when the Sifting Process is applied to the data of Figure 3(g) without applying the intermittency test option;

Figures 3(k)-(m) are graphs of the first, second, and third intrinsic mode functions when the Sifting Process is applied to the data of Figure 3(g) which applies the intermittency test option.

Figure 4(a) is a graph of a wind speed signal which is for explaining the computer implemented Empirical Mode Decomposition method of the invention;

Figures 4(b)-(k) show the wind speed signal and the nine intrinsic mode functions which are extracted from the wind speed signal by the EMD method of the invention;

Figures 5(a)-(j) are a series of graphs illustrating the successive reconstruction of the original wind speed data from the intrinsic mode functions;

Figure 6(a) is the Hilbert Spectrum generated by the invention from the wind speed data of Figure 4(a);

Figure 6(b) is the conventional Morlet Wavelet spectrum generated from the wind speed data of Figure 4(a);

Figure 6(c) shows the Hilbert Spectrum of Figure 6(a) after smoothing by a 15x15 weighted Gaussian smoothing filter;

Figure 7 is a comparison of the marginal Hilbert spectrum (solid line) and the Fourier spectrum (dotted line) which were generated from the wind speed signal of Figure 4(a);

Figure 8(a) is a graph illustrating the Degree of Stationarity and Degree of Statistical Stationarity which were generated from the wind speed signal of Figure 4(a) with time averages of 10, 50, 100 and 300; Figures 8(b) and (c) are sections of the wind speed data that was used by the invention to produce the Degree of Stationarity shown in Figure 8(a);

Figures 9(a)-(d), (f) and (g) are graphs of blood pressure data taken from the pulmonary artery of an normal, active rat which provide examples of biological data that may be processed by the invention;

Figure 9(e) shows an envelope linking the systolic pressure extrema values for explaining the concepts of the invention;

Figure 10(a) shows a conventional Fourier Spectrum (energy versus frequency) of the blood pressure data from Figure 9(b) for illustrating advantages of the invention;

Figures 10(b)-(c) show conventional Fourier Spectrums (energy versus frequency) of the blood pressure data from Figures 9(c)-(d) for further illustrating advantages of the invention;

Figure 10(d) shows a conventional Fourier Spectrum (time versus frequency) of the blood pressure data from Figure 9(b) for illustrating advantages of the invention;

Figures 10(e)-(f) show conventional three-dimensional Fourier Spectrum (amplitude of spectrum as a function of frequency in every 1-minute window on the time-frequency plane

in linear scales) of the blood pressure data from Figure 9(b) for illustrating advantages of the invention;

Figure 10(g) is a combined graph directly comparing a conventional Fourier Spectrum and a marginal Hilbert Spectrum according to the invention calculated from the data of Figure 9(c);

Figures 11(a)-(h) are graphs of the first through eighth intrinsic mode functions which are extracted from the blood pressure signal of Figure 9(c) by the EMD method of the invention;

Figures 12(a)-(h) are graphs of the first through eighth intrinsic mode functions which are extracted from the blood pressure signal of Figure 9(d) by the EMD method of the invention;

Figures 13(a) and (b) are reconstructions of the blood pressure signal of Figure 9(d) based on subsets of the intrinsic mode functions;

Figure 13(c) is another reconstructions of the blood pressure signal of Figure 9(d) based on a different subset of the intrinsic mode functions plotted together with the original signal (dotted line) of Figures 9(d);

Figure 14(a) is a Hilbert Spectrum of the Figure 9(d) blood pressure signal calculated according to the invention;

Figure 14(b) is a Hilbert Spectrum of the Figure 9(c) blood pressure signal calculated according to the invention;

Figures 15(a)-(d) are graphs of pulmonary blood pressure signals in response to step changes in oxygen concentration in the breathing gas;

Figures 15(e)-(h) illustrate the inventive sifting process as it is applied to the data of Figures 15(b);

Figures 16(a)-(p) are graphs of the first through sixteenth intrinsic mode functions which are extracted from the blood pressure signal of Figure 15(a) by the EMD method of the invention;

Figures 17(a)-(f) are mean trends of pulmonary arterial blood pressure which are computed according to the invention;

Figures 18(a)-(c) are analytic functions derived by the invention and representing the indicial response of pulmonary arterial blood pressure to a step decrease in oxygen concentration from 20.9 to 10.0%;

Figures 19(a)-(c) are analytic functions derived by the invention and representing the indicial response of pulmonary arterial blood pressure to a step increase in oxygen concentration from 10.0 to 20.9%;

Figures 20(a)-(d) are oscillations about the mean trend as defined by the invention for $k=1, 2, 4$ and 6 , respectively;

Figure 21 shows the Hilbert energy spectrum $E_k(t)$ according to the invention which is calculated from the instantaneous amplitude spectrum of the oscillations about the mean $X_k(t)$ with $k=6$ (the data from Figure 20(d));

Figures 22(a)-(h) are graphs of the first through sixteenth intrinsic mode functions which are extracted from the Hilbert energy spectrum $E_k(t)$ of Figure 21 by the EMD method of the invention;

Figures 23(a)-(b) show the three dimensional (amplitude-frequency-time) and two-dimensional (contour of amplitude on the frequency-time plane) plot of the Hilbert Spectrum (HHT) taken from the data of Figure 20(d);

Figure 24 shows a conventional two dimensional Fourier Spectrum (FFT) of the pressure signal in 1-minute segments under the assumption that the process is stationary in each segment;

Figure 25 is a graph of heart pulse interval versus time taken from a human with sleep apnea and including both a normal and abnormal (apnea) data section;

Figure 26 is a graph of a normal heart pulse interval versus time;

Figures 27(a)-(h) are graphs of the first through seventh intrinsic mode functions and the residue which are extracted from the normal heart pulse interval data of Figure 26 by the EMD method of the invention;

5 Figure 28 is a blow up of Figure 26;

Figure 29 is a Hilbert Spectrum of the Figure 26 normal heart pulse interval data calculated according to the invention;

10 Figure 30 is a graph of an abnormal heart pulse interval versus time;

Figures 31(a)-(h) are graphs of the first through seventh intrinsic mode functions and the residue which are extracted from the abnormal heart pulse interval data of Figure 29 by the EMD method of the invention;

5 Figure 32 is a blow up of Figure 30;

Figure 33 is a Hilbert Spectrum of the Figure 30 abnormal heart pulse interval data calculated according to the invention;

20 Figure 34 is heart pulse rate data for 45 minute interval during which the patient suffered an epileptic seizure (at time index 0);

25 Figures 35(a)-(i) are graphs of the first through ninth intrinsic mode functions which are extracted from the heart pulse interval data of Figure 34 by the EMD method of the invention;

Figures 36(a)-(c) are the first intrinsic mode function , the original heart pulse interval data, and the third intrinsic mode function of the Figure 34 epileptic seizure data plotted on an expanded scale, respectively;

30 Figure 37 is a Hilbert Spectrum of the Figure 34 epileptic seizure, heart pulse interval data calculated according to the invention; and

Figure 38 is a conventional Wavelet Spectrum of the Figure 34 epileptic seizure, heart pulse interval data for comparison with the inventive result of Figure 37.

Figure 39 is a block diagram describing the inventive method of speech analysis.

Figure 40 is a block diagram describing the inventive method of speech synthesis.

Figure 41 is a block diagram describing the inventive method of speaker identification.

Figure 42 is a block diagram describing the inventive method of speech recognition.

Figure 43 is a block diagram describing the inventive method of sound quality enhancement.

Figure 44 is a block diagram describing the inventive method of machine health monitoring.

Figure 45(a) shows acoustical signal data recorded from a male speaker, saying 'Halloo.'

Figure 45(b) shows acoustical signal data recorded from a female speaker, saying 'Halloo.'

Figure 46(a)-(b) show the EMD decomposed IMF components of Figure 45(a)-(b).

Figure 47(a)-(b) show the Hilbert Spectra of Figure 46(a)-(b).

Figure 48(a)-(b) show the Fourier Spectra of Figure 46(a)-(b).

Figure 49(a)-(b) show the detailed Hilbert Spectra of Figure 46(a)-(b).

Figure 50 shows the wide banded Fourier Spectrogram of Figure 45(a), constructed from 128 sampled points.

Figure 51(a)-(b) show the detailed Fourier Spectrogram of Spectra of Figure 46(a)-(b).

Figure 52(a)-(b) show the detailed Morlet Wavelet Spectra of Figure 46(a)-(b).

Figure 53(a)-(b) show the detailed Hilbert Spectra of Figure 49(a)-(b).

Figure 54(a)-(b) show the detailed Hilbert Spectra and the acoustical signal data of Figure 46(a)-(b).

Figure 55 shows the acoustical signal data of the sounds, "Halloo + Ding," "Halloo," and "Ding," respectively.

Figure 56(a) shows the EMD decomposed IMF components of sound "Halloo + Ding", wherein each of the components is plotted in the uniform vertical scale.

Figure 56(b) shows the EMD decomposed IMF components of sound "Halloo + Ding", wherein each of component is plotted in the vertical scale normalized within its own frame.

Figure 57(a) shows the filtered IMF components of the sound "Halloo + Ding", wherein the signal associated with the sound "Ding" has been eliminated.

Figure 57(b) shows the IMF components of the sound "Ding," separated from Figure 56(a).

Figure 58(a) shows the Hilbert Spectrum of the sound "Halloo + Ding."

Figure 58(b) shows the HHT filtered Hilbert Spectrum of the sound "Halloo + Ding."

Figure 59(a) shows the acoustical signal data, filtered with HHT and Fourier, respectively.

Figure 59(a) shows Fourier Spectra for the sound "Halloo + Ding" and various filtered data.

Figure 60(a)-(c) show the acoustical data from a grinder operating on a hard surface continuously for 95, 120, and 200 hours, respectively.

Figure 61(a)-(c) show the EMD decomposed IMF components of Figure 60(a)-(c).

Figure 62(a)-(c) show the Hilbert Spectra of Figure 60(a)-(c).

DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

Before describing the computer implemented Empirical Mode Decomposition method in detail and its application to biological data and acoustical data, the definition and physical meaning of intrinsic mode functions in general will be discussed.

Intrinsic Mode Function

An Intrinsic Mode Function (IMF) is a function that satisfies the following two conditions:

- (a) in the whole data set, the number of extrema and the number of zero-crossings must either be equal or differ at most by one, and
- (b) at any point, the mean value of upper envelope defined by the maxima and the lower envelope defined by the minima is zero.

The first condition shares some similarity to the traditional narrow band requirements for a stationary Gaussian process. The second condition is a totally new idea. Conceptually, the second condition modifies the classical global requirement to a local one. Furthermore, the second condition has the desirable result that the instantaneous frequency will not have unwanted fluctuations induced by asymmetric wave forms. Mathematically, the second condition should ideally be 'the local mean of the data being zero.'

For nonstationary data, the 'local mean' requires a 'local time scale' to compute the mean, which is impossible to define. Fortunately, the local time scale need not be defined to fulfil the second condition, as will be discussed below.

To apply these concepts to physical data, the invention utilizes the local mean of the signal envelopes to force the local symmetry.

The signal envelopes are defined by the local maxima and the local minima. This is an approximation which avoids the definition of a local averaging time scale.

With the physical approach and the approximation adopted here, the inventive method does not always guarantee a perfect instantaneous frequency under all conditions. Nevertheless, it can be shown that, even under the worst conditions, the instantaneous frequency so defined is still consistent with the physics of the system being studied and represents the system being studied much more accurately than previous techniques based on Fourier analysis.

The term "Intrinsic Mode Function" is adopted because it represents the oscillation mode embedded in the data. With this definition, the IMF in each cycle, defined by the zero-crossings, involves only one mode of oscillation. In other words, each IMF represents only one group of oscillation modes or time scales and no riding waves are allowed.

Before presenting the inventive EMD method for decomposing the data into IMFs, a qualitative assessment of the intrinsic oscillatory modes may be roughly determined by simply examining the data by eye. From this examination, one can immediately identify the different scales directly in two ways: the time lapse between the successive alternations of local maxima and minima and the time lapse between the successive zero-crossings reveals the different scales. The interlaced local extrema and zero-crossings give us complicated data: one undulation is riding on top of another, and they, in turn, are riding on still other undulations, and so on. Each of these undulations defines a characteristic scale or oscillation mode that is intrinsic to the data: hence, the term "Intrinsic Mode Function" is adopted.

To reduce the data into the needed IMFs, the invention utilizes a computer implemented Empirical Mode Decomposition Method which is described below.

Empirical Mode Decomposition (EMD): The Sifting Process

First, the Empirical Mode Decomposition method which deals with both nonstationary and nonlinear data will be

discussed. Then, the physical meaning of this decomposition will be presented.

The essence of the EMD method is to identify empirically the intrinsic oscillatory modes by their characteristic time scales in the data, and then decompose the data accordingly. The decomposition is based on the following assumptions:

- a. the signal has at least two extrema: one maximum and one minimum, and
- b. the characteristic time scale is defined by the time lapse between the extrema.

In other words, the invention adopts the time lapse between successive extrema as the definition of the time scale for the intrinsic oscillatory mode because it gives a much finer resolution of the oscillatory modes and because it can be applied to data with non-zero mean (either all positive or all negative values, without zero-crossings). A systematic way to extract the intrinsic mode functions is the computer implemented Empirical Mode Decomposition method or Sifting Process which is described as follows.

Figure 1(a) illustrates the overall inventive method including the Sifting Process in step 120. First, the physical activity, process or phenomenon is sensed by an appropriate sensor in step 100. Appropriate sensors for detecting the physical activity and generating a physical signal representative thereof are discussed in the practical examples below. As an equivalent alternative, the physical signal can be inputted in step 100.

After sensing in step 100, the analog signal is converted to the digital domain suitable for computer processing in the A/D conversion step 105. Depending upon whether the input signal is analog or digital step 105 may be bypassed.

Next, an optional smoothing step 110 may be applied to the physical signal. The optional smoothing step 110 may be

applied to smooth the signal with, for example, a weighted running average to remove excessive noise.

Thereafter, the Sifting Process is applied in step 120 to Sift the signal with the Empirical Mode Decomposition method and thereby extract the intrinsic mode function(s). The intrinsic mode functions can then be displayed as shown in step 130 and checked for orthogonality in step 135.

Before continuing with the main flow in Figure 1(a), the details of the Sifting Process will be explained with reference to the high level flowchart in Figures 2(a), 2(b) and the series of graphs showing illustrative results of the Sifting Process in Figures 3(a)-(f).

As shown in Figure 1(b), the digitized physical signal from step 105 is first windowed by framing the end points in step 107. Then, the Sifting Process begins at step 200 by identifying local maximum values of the digitized, framed physical signal from step 107. Figure 3(a) shows a typical physical signal 10 which, in this example, represents wind speed spanning a time interval of one second.

Before construction of the envelope in steps 210 and 230, optional intermittency tests (201,221) may be introduced to alleviate the alias associated with intermittence in the data that can cause mode mixing.

Optional intermittency test 201 checks the distance between successive maxima to see if this distance between is within a pre-assigned value n times the shortest distance between waves. If no, then an intermittency exists and the method proceeds to step 202. If yes, then there is no intermittency and the upper envelope is constructed in step 210 as further described below.

Similarly optional intermittency test 221 checks the distance between successive minima to see if this distance is within a pre-assigned value n times the shortest distance between waves. If no, then an intermittency exists and the

method proceeds to step 222. If yes, then there is no intermittency and the upper envelope is constructed in step 230 as further described below.

An example of such intermittency is given in Figure 3(g), in which small scale waves appear only intermittently. By strict application of the Sifting Process, the resulting IMFs are given in Figures 3(b)-(j), in which two drastically different time scales are present in the first IMF component as shown in Figure 3(h). This mixing of modes breaks up the main wave train by the small intermittent oscillations.

If intermittency tests (201,222) are employed which utilize a preassigned value of n-times the shortest distance between waves, the resulting IMFs are shown in Figures 3(k)-(m), in which the modes are clearly and physically separated. The effective step to eliminate the mode mixing is achieved by treating the local extrema which failed the intermittency test as local maxima and minima (steps 202 and 212), respectively. Therefore, the upper and lower envelope will be identical as the original data reference line.

These intermittency tests (201,221) and the further steps (202,222) are optional. By selecting an artificially large n value utilized in steps 201 and 221 to test for intermittency, the test will be effectively bypassed. Otherwise, the test can be bypassed at the initial selection of the program.

Then, the method constructs an upper envelope 20 of the physical signal 10 in step 210. The upper envelope 20 is shown in Figure 3(b) using a dot-dashed line. This upper envelope 20 is preferably constructed with a cubic spline that is fitted to the local maxima.

Next, the local minimum values of the physical signal 10 are identified in step 220. To complete the envelope, a lower envelope 30 is constructed from the local minimum values in step 230. The lower envelope 30 is also shown in Figure 3(b) using a dot-dash line. Like the upper envelope 20, the lower

envelope 30 is preferably constructed with a cubic spline that is fitted to the local minima.

The upper and lower envelopes 20, 30 should encompass all the data within the physical signal 10. From the upper and lower envelopes 20, 30, an envelope mean 40 is determined in step 240. The envelope mean 40 is the mean value of the upper and lower envelopes 20, 30. As can be seen in Figure 3(b), the envelope mean 40 bisects the physical signal 10 quite well.

Then, the method generates the first component signal h_1 in step 250 by subtracting the envelope mean 40 from the physical signal 10. This computer implemented step may also be expressed as:

$$X(t) - m_1 = h_1 \dots 1$$

Where the envelope mean 40 is m_1 and the physical signal is $X(t)$.

Figure 3(c) shows the first component signal h_1 . Ideally, the first component signal h_1 should be an IMF, for the construction of h_1 described above seems to have made h_1 satisfy all the requirements of an IMF. In reality, however, a gentle hump that resides on a slope region of the data can become an extremum when the reference coordinate is changed from the original rectangular coordinate to a curvilinear coordinate. For example, the imperfection of the envelopes 20, 30 can be seen by observing the overshoots and undershoots at the 4.6 and 4.7 second points in Figure 3(b).

An example of this amplification can be found in the gentle hump between the 4.5 and 4.6 second range in the data in Figure 3(a). After the first round of sifting, the gentle hump becomes a local maximum at the same time location in the first component signal h_1 shown in Figure 3(c). New extrema generated in this way actually recover the proper modes lost

in the initial examination. Thus, the Sifting Process extracts important information from the signal which may be overlooked by traditional techniques. In fact, the Sifting Process can recover low amplitude riding waves, which may appear as gentle humps in the original signal, with repeated siftings.

Still another complication is that the envelope mean 40 may be different from the true local mean for nonlinear data. Consequently, some asymmetric wave forms can still exist no matter how many times the data are sifted. This must be accepted because, after all, the inventive method is an approximation as discussed before.

Other than these theoretical difficulties, on the practical side, serious problems of the spline fitting can occur near the ends, where the cubic spline being fit can have large swings. Left by themselves, the end swings can eventually propagate inward and corrupt the whole data span especially in the low frequency components. A numerical method has been devised to eliminate the end effects details of which will be given later. Even with these problems, the Sifting Process can still extract the essential scales from the data.

The Sifting Process serves two purposes: to eliminate riding waves and to make the wave profiles more symmetric. Toward these ends, the Sifting Process has to be repeated. Because only the first component signal h_1 has been generated so far, the decision step 260, which tests successive component signals to see if they satisfy the definition of an IMF, is bypassed during the first iteration.

Thus, step 265 is performed which treats the component signal as the physical signal in the next iteration. The next iteration is then performed by executing steps 200-250. In step 250, the second component signal h_{11} is generated by subtracting the envelope mean from the physical signal (in

this iteration, the first component signal h_1 is treated as the physical signal). In more formal terms:

$$h_1 - m_{11} = h_{11} \dots\dots 2$$

Figure 3(d) shows the second component signal h_{11} .

Although the second sifting shows great improvement in the signal with respect to the first sifting, there is still a local maximum below the zero line. After a third sifting, the result (third component signal h_{12}) is shown in Figure 3(d). Now all the local maxima are positive, and all the local minima are negative, but to ensure this configuration is stable, the Sifting Process should be further repeated. In general, the Sifting Process is repeated at least 3 more times and, in general, K times to produce h_{1k} . If no more new extrema are generated, then h_{1k} is an IMF. In formal terms:

$$h_1(k-1) - m_{1k} = h_{1k} ; \dots 3$$

The resulting first IMF component is shown in Figure 3(f) after 9 siftings. The first IMF component of the physical signal may be designated as such in step 270 and stored in step 275 in memory 415:

$$c_1 = h_{1k} , 4$$

As mentioned above, all these manipulations are carried out numerically in a computer 410. There is not explicit close form analytic expression for any of the computer implemented steps.

As described above, the process is indeed like sifting of the data by the computer 410 because it separates the finest (shortest time scale) local mode from the data first based only on the characteristic time scale. The Sifting Process, however, has two effects:

- a. to eliminate riding waves, and
- b. to ensure the envelopes generated by maxima and minima are symmetric.

While the first condition is necessary for the instantaneous frequency to be meaningful (as discussed below), the second condition is also necessary in case the neighboring wave amplitudes have too large a disparity.

Unfortunately, the effects of the second condition, when carried to the extreme, could obliterate the physically meaningful amplitude fluctuations. Therefore, the Sifting Process should be applied with care, for carrying the process to an extreme could make the resulting IMF a pure frequency modulated signal of constant amplitude.

To guarantee that the IMF component retains enough physical sense of both amplitude and frequency modulations, a stopping criterion is employed to stop the generation of the next IMF component.

This stopping criterion is part of the computer implemented method and is shown as step 260 in Figure 1(c). Step 260 is a decision step that decides whether the stopping criteria has been satisfied. The preferred stopping criteria determines whether three successive component signals satisfy the definition of IMF. If three successive component signals all satisfy the definition of IMF, then the Sifting Process has arrived at an IMF and should be stopped by proceeding to step 270. If not, step 260 starts another iteration by proceeding to step 265 as described above.

Alternatively, another stopping criteria could be used that determines whether successive component signals are substantially equal. If successive component signals are substantially equal, then the Sifting Process has arrived at an IMF and should be stopped by proceeding to step 270. If not, step 260 starts another iteration by proceeding to step 265 as described above.

Determining whether successive component signals are substantially equal in the alternative stopping criteria limits the size of the standard deviation, **sd**, computed from the two consecutive sifting results as follows:

$$sd = \frac{T}{\Delta} \left[\frac{\Omega(h_1(k-1)(t) - h_{1k}(t))\Omega^2}{2h_1(k-1)(t)} \right] .5$$

5 A very rigorous and preferred value for **sd** is set between 0.2 and 0.3. Of course, if faster processing is desired, then a trade-off such as a less rigorous value for **sd** may be used.

Overall, the first IMF component **c₁** should contain the finest scale or the shortest period component of the physical signal 10.

Before extracting the next IMF component, a test should be conducted to determine if the Sifting Process should stop. The stopping criteria is shown in Step 300. Step 300 determines whether the component signal has more than 2 extrema. If not, all of the IMF's have been extracted and the Sifting Process is stopped by proceeding to step 310. If so, then additional IMF's may be extracted by continuing the process in step 320.

Step 270 recognizes that an IMF component has been successfully generated by the Sifting Process by setting the component signal equal to an intrinsic mode function. More specifically, step 270 causes the computer 410 to store the component signal **h_{1k}** as an intrinsic mode function in memory 415.

25 Then, the first IMF is separated from the physical signal in step 290 to generate a residual signal. In particular, a residual signal is generated by subtracting the intrinsic mode function from the physical signal. In formal terms:

$$X(t) - c_1 = r_1 .6$$

Because the residue, r_1 , still includes information of longer period components, it is treated as the new physical data and subjected to the same Sifting Process as described above. Step 320 performs this function by treating the residual signal as the physical signal in the next iteration. Thereafter, the next iteration is performed beginning with the execution of step 200 as described above.

The Sifting Process is analogous to a mechanical sieve, except it is implemented here in specially programmed computer and applied to any digital data numerically rather than mechanically.

The Sifting Process is repeated for all the subsequent r_j 's. This iterative procedure may be expressed as:

$$\begin{array}{l} r_1 - c_2 = r_2 , \\ \quad \quad \quad \diamond\diamond\diamond, \quad \quad \quad 7 \\ r_{n-1} - c_n = r_n . \end{array}$$

Step 300 stops the Sifting Process by proceeding to stop step 310 if the residual signal r_n has more than 2 extrema. Otherwise, the method proceeds to step 320.

In other words, Step 310 stops the Sifting Process if the residual signal r_n is monotonically increasing or decreasing. This stopping criterion is based on the fact that an IMF cannot be extracted from a monotonic function. If r_n is not monotonically increasing/decreasing, then a next iteration is performed beginning with step 320.

Even for data with zero mean, the final residue still can be different from zero. For data with a trend, the final residue should be that trend.

In summary, the Sifting Process decomposes the physical signal $X(t)$ into a series of intrinsic mode functions and a residue which may be expressed as:

$$X(t) = \sum_{i=1}^n c_i + r_n \cdot 8$$

In other words, the invention extracts a series of IMFs by Sifting the physical signal with a computer implemented Empirical Mode Decomposition method. This IMF series cannot be generated or derived by any analytic method. It can only be extracted by the invention through a specially programmed computer through the Sifting Process.

EMD Filtering and Curve Fitting

Figure 1(d) illustrates the inventive method of performing filtering and curve fitting. The method begins, as in Figure 1(a), with sensing the physical phenomenon or inputting a signal representative thereof in step 100. The optional smoothing 105 may then be applied to eliminate excess noise.

Then, the signal is Sifted with the Empirical Mode Decomposition Process to extract the intrinsic mode functions in step 120. The IMFs may then be directly displayed 130, stored 132 or transmitted 134.

As mentioned above, fitting a curve to a signal is not always possible. The reasons include too many data points for efficient curve fitting and nonlinear data that does not admit an acceptable curve fit. The IMFs, however, extract important information from the original signal while reducing the number of data points and simplifying the resulting signal. By properly selecting only the most relevant IMFs, one can construct a filtered version of the original signal.

Step 350 performs this process of constructing a filtered signal from a subset of the IMFs. Selecting which IMFs should in the subset and which should not may be an empirical or intuitive process. Typically, the IMFs having the lowest frequency components are chosen as part of the selected subset with the higher frequency components excluded therefrom. In this way, a simplified (filtered) version of the original signal can be constructed which eliminates unnecessary and, hopefully, not physically components (IMFs).

More specifically, step 350 performs a summation of the selected IMFs. The selection of IMFs can be automated, e.g. the n lowest frequency IMFs, or manual.

Generating the filtered signal typically permits curve fitting to be successful and efficient. Once the filtered signal is generated, conventional curve fitting techniques (step 360) such as a least squares estimation process can be utilized.

The fitted curve may then be outputted 362, displayed 364, stored 366 or transmitted 368.

The filtered signal may also be subjected to further processing in step 370. Namely, the oscillatory energy about the mean is calculated in step 370. This calculation is essentially the same as the instantaneous energy density calculation explained below, with the calculation being performed for a subset (k) of the IMFs. Further details and an example are discussed below. The result of step 370 is a signal that may be subjected to the Sifting Process to extract a set of IMFs in step 120. Although Figure 1(d) illustrates an infinite loop (steps 120, 350 and 370), at some point it will not be appropriate or possible extract further IMFs. Thus, this loop is not really infinite and is typically performed one or two times.

Computer for Implementing Inventive Method

A computer suitable for programming with the inventive method is diagrammatically shown in the block diagram of Figure 2. The computer 410 is preferably part of a computer system 400. To allow human interaction with the computer 410, the computer system includes a keyboard 430 and mouse 435. The computer programmed with the inventive method is analogous to a mechanical sieve: it separates digital data into series of IMF's according to their time scales in a manner analogous to a mechanical sieve which separates aggregated sand particles according to their physical size.

Because the invention is applied to analyze physical signals, the computer system 400 also includes an input device 440, sensor 442 and/or probe 444 which are used to sample a physical phenomenon and generate physical signal representative thereof. More particular examples of such inputs (440, 442 and 444) are described in relation to Figures 21-25.

To output the results of the computer implemented method, the computer system 400 also includes a display 450 such as a cathode ray tube or flat panel display, printer 460 and output device 470. Each of these outputs (450, 460, 470) should have the capability to generate or otherwise handle color outputs because, for example, the Hilbert Spectrum may be in color.

The generalized output device 470 may also include a network connection to connect the computer 400 to a local or wide area network. In this way, the physical signal may be inputted from the network. Furthermore, all outputs can be sent to another location via such a network connection.

Furthermore, the computer system 400 also includes a mass storage device 420. The mass storage device 420 may be a hard disk, floppy disc, optical disc, etc. The mass storage device 420 may be used to store a computer program which performs the invention when loaded into the computer 410. As an alternative, the input device 440 may be a network connection

or off-line storage which supplies the computer program to the computer 410.

More particularly, the computer program embodiment of the invention may be loaded from the mass storage device 420 into the internal memory 415 of the computer 410. The result is that the general purpose computer 410 is transformed into a special purpose machine that implements the invention.

Even more particularly, each step of inventive method will transform at least a portion of the general purpose computer 410 into a special purpose computer module implementing that step. For example, when the sifting step 120 is implemented on the computer 410, the result is a computer implemented sifting apparatus (sifter) that performs the sifting functions of sifting step 120.

Other embodiments of the invention include firmware embodiments and hardware embodiments wherein the inventive method is programmed into firmware (such as EPROM, PROM or PLA) or wholly constructed with hardware components. Constructing such firmware and hardware embodiments of the invention would be a routine matter to one of ordinary skill using known techniques.

Article of Manufacture

Still further, the invention disclosed herein may take the form of an article of manufacture. More specifically, the article of manufacture is a computer-usable medium, including a computer-readable program code embodied therein wherein the computer-readable code causes computer 410 to execute the inventive method.

A computer diskette such as disc 480 in Figure 2 is an example of such a computer-usable medium. When the disc 480 is loaded into the mass storage device 480, the computer-readable program code stored therein is transferred into the

computer 410. In this way, the computer 410 may be instructed to perform the inventive methods disclosed herein.

Illustration of Sifting Process

5 To further illustrate the Sifting Process, consider Figure 4(a) which shows a physical signal representing wind data collected in a laboratory wind-wave tunnel with a high frequency response Pitot tube located 10 cm above the mean water level. The wind speed was recorded under the condition of an initial onset of water waves from a calm surface. Clearly, the physical signal is quite complicated with many local extrema but no zero-crossings such that the time series represents all positive numbers.

10 Although the mean can be treated as a zero reference, defining it is difficult, for the whole process is transient. This example illustrates the advantage of adopting the successive extrema for defining the time scale and the difficulties of dealing with nonstationary data. In fact, a physically meaningful mean for such data is impossible to define using standard methods. The EMD eliminates this difficulty.

15 Figure 4(b) shows the wind speed signal of Figure 4(a) on a different scale for comparison purposes. Figures 4(c)-(k) show all the IMFs obtained from repeatedly sifting the wind speed signal in Figure 4(b). The efficiency of the invention is also apparent: the Sifting Process produces a total of 9 intrinsic mode function components while the Fourier transform needs components which number as many as half of the total number of points in a given window to represent the wind data with the same accuracy.

20 The separation of the wind speed data into locally non-overlapping time scale components is clear from Figures 4(c)-(k). In some components, such as c_1 and c_3 , the signals are intermittent, then the neighboring components might include

oscillations of the same scale, but signals of the same time scale would never occur at the same locations in two different IMF components.

5 The components of the EMD are usually physical, for the characteristic scales are physically meaningful.

10 To confirm the validity and completeness of the Sifting Process, the wind speed signal can be reconstructed from the IMF components. Figures 5(a)-(i) show this reconstruction process starting from the longest period IMF to the shortest period IMF in sequence. For example, Figure 5(a) shows the wind speed signal and the longest period component, c_9 , which is actually the residue trend, not an IMF.

5 By itself, the fitting of the trend is quite impressive, and it is very physical: the gradual decrease of the mean wind speed indicates the lack of drag from the calm surface initially and the increasing of drag after the generation of wind waves. As the mean wind speed decreases, the amplitude of the fluctuation increases, another indication of wind-wave interactions.

20 By adding the next longest period component, c_8 , the trend of the sum, $c_9 + c_8$, takes a remarkable turn, and the fitting to the wind speed signal looks greatly improved as shown in Figure 5(b). Successively adding more components with increasing frequency results in the series of Figures 5(c)-(i). The gradual change from the monotonic trend to the final reconstruction is illustrative by itself. By the time the sum of IMF components reaches c_3 in Figure 5(g), essentially all the energy contained in the wind speed signal is recovered. The components with the highest frequencies add little more
25 energy, but they make the data look more complicated. In fact, the highest frequency component is probably not physical, for the digitizing rate of the Pitot tube is too slow to capture the high frequency variations. As a result, the data are jagged artificially by the digitizing steps at
30

this frequency. The difference between the original data and the re-constituted set from the IMF's is given in Figure 5(j). The magnitude of the difference is 10^{-15} , which is the limit of the computer 410.

5

The Hilbert Spectrum

Having obtained the Intrinsic Mode Function components (through either the local extrema or curvature extrema Sifting Processes), the next step in the computer implemented method is to apply the Hilbert Transform to each component and generate the Hilbert Spectrum as shown in step 140 in Figure 1(a). A brief tutorial on the Hilbert transform with emphasis on its physical interpretation can be found in Bendat and Piersol, 1986, *"Random Data: Analysis and Measurement Procedures"*, 2nd Ed., John Wiley & Sons, New York, NY. Essentially, the Hilbert transform is the convolution of $\mathbf{X}(t)$ with $1/t$. This convolution emphasizes the local properties of $\mathbf{X}(t)$. In more formal terms, given a time series $\mathbf{X}(t)$, the Hilbert Transform $\mathbf{Y}(t)$ can be expressed as

$$Y(t) = \frac{1}{P} \int_{-\infty}^{\infty} \frac{X(t\phi)}{t-t\phi} dt\phi \quad 9$$

20 where P indicates the Cauchy principal value.

With this definition, $\mathbf{X}(t)$ and $\mathbf{Y}(t)$ form a complex conjugate pair. This complex conjugate pair $\mathbf{Z}(t)$ may be expressed as:

$$Z(t) = X(t) + iY(t) = a(t) e^{iq(t)}, \quad 10$$

25 in which

$$a(t) = [X^2(t) + Y^2(t)]^{1/2}, \quad 11$$

$$q(t) = \arctan \frac{Y(t)}{X(t)}. \quad 12$$

After performing the Hilbert transform to each IMF component, we can express the time series data $\mathbf{x}(t)$ in the following form:

$$X(t) = \sum_{j=1}^n a_j(t) e^{i \int w_j(t) dt} \quad .13$$

In Equation (13), the residue, r_n , is purposefully omitted, for it is either a monotonic function, or a constant. Although the Hilbert transform can treat the monotonic trend as part of a longer oscillation, the energy involved in the residual trend could be overpowering. In consideration of the uncertainty of the longer trend, and in the interest of information contained in the other low energy and higher frequency components, the final non-IMF component should be left out. It, however, could be included, if physical considerations justify its inclusion.

Note that Equation (13) gives both amplitude and frequency of each component as functions of time. It should be pointed out that no analytical method can generate the expression in Equation (13). Instead, all the components may be extracted only by a specially programmed computer applying the inventive Sifting Process and the Hilbert transform. The variable amplitude and frequency have not only greatly improved the efficiency of the expansion, but also enabled the expansion to accommodate nonstationary data. With IMF expansion, the amplitude and the frequency modulations are also clearly separated.

Equation (13) also enables the computer implemented method to represent the amplitude and frequency as functions of time in a three-dimensional plot, in which the amplitude can be contoured on the frequency-time plane. This frequency-

time distribution of the amplitude is designated as the Hilbert Amplitude Spectrum, $H(_, t)$, or simply Hilbert Spectrum. Thus we have:

$$H(w, t) = \sum_{j=1}^n \hat{a}_j(t) e^{i\int w_j(t) dt} \dots\dots\dots 14$$

5 In which $H(_, t)$ is the Hilbert spectrum of the frequency ($_$) and time (t) and $a_j(t)$ is the j -th component of the IMF.

In the presentation, the amplitude (with or without smoothing) can be expressed in color maps, black-grey maps, or contour maps. Color maps, however, greatly increase the operator's ability to fully analyze the spectrum. In some cases, a color map will permit the operator to discern relationships and trends that would not be apparent in black-grey maps thereby making a color display a necessary component in some cases.

If amplitude squared is more desirable to represent energy density, then the squared values of amplitude can be substituted to produce a Hilbert Energy Spectrum just as well.

Various forms of Hilbert spectra presentations can be generated by the computer in the display step 190: both color
20 coded maps and contour maps may be employed to present the Hilbert spectra with or without smoothing. The Hilbert Spectrum in the color map format for the wind data is shown in Figure 6(a). The Hilbert spectrum in Figure 6(a) gives a very different appearance when compared with the corresponding
25 Wavelet spectrum shown in Figure 6(b). While the Hilbert Spectrum in Figure 6(a) appears only in the skeleton form with emphasis on the frequency variations of each IMF, the Wavelet analysis result gives a smoothed energy contour map with a rich distribution of higher harmonics.

30 If a more continuous form of the Hilbert Spectrum is preferred, a smoothing method can be optionally applied in

step 155. The first type of a smoothing method which may be used in the invention is a weighted spatial filter which averages over a range of cells. For example, a 15 by 15 weighted Gaussian filter may be employed in step 155 as is known in the art to smooth this data. Figure 6(c) shows the result of applying the 15 by 15 weighted Gaussian filter.

Although smoothing step 155 degrades both frequency and time resolutions, the energy density and its trends of evolution as functions of frequency and time are easier to identify. In general, if more quantitative results are desired, the original skeleton presentation is better. If more qualitative results are desired, the smoothed presentation is better. As a guide, the first look of the data is better in the smoothed format.

The alternative of the spatial smoothing is to select a lower frequency resolution and leave the time axis undisturbed. The advantages of this approach are the preservation of events' locations and a more continuous frequency variation. Furthermore, a lower frequency resolution saves computation time for the computer implemented method.

To optimize such computation time, the optimal frequency resolution in the Hilbert spectrum can be computed as follows. Let the total data length be T , and the digitizing rate of the sensor be Δt . Then, the lowest frequency that can be extracted from the data is $1/T$ Hz, which is also the limit of frequency resolution for the data. The highest frequency that can be extracted from the data is $1/(n \Delta t)$ Hz, in which n represents the minimum number of Δt needed to define the frequency accurately.

Because the Hilbert transform defines instantaneous frequency by differentiation, more data points are needed to define an oscillation. The absolute minimum number of data points is five for a whole sine wave. Although a whole sine

wave is not needed to define its frequency, many points within any part of the wave are needed to find a stable derivative. Therefore, the maximum number of the frequency cells, N , of the Hilbert spectrum should be

$$N = \frac{1}{\frac{nDt}{1}} = \frac{T}{nDt} \quad .15$$

5

In order to make the derivative stable, the data is averaged over three adjacent cell values for the final presentation.

To illustrate, consider the wind data of Figure 4(a) which was digitized at a rate of 0.01 seconds and has a total length of 30 seconds. Therefore, the highest frequency that can be extracted is 25 Hz. The total cell size could be 600, but they have been averaged to 200 in Figure 6(a).

Marginal Spectrum

The marginal spectrum offers a measure of total amplitude (or energy) contribution from each frequency value. In other words, the marginal spectrum represents the cumulated amplitude over the entire data span.

20 As shown in Figure 1(a), the marginal spectrum is calculated by the computer implemented method in step 145 after applying the Hilbert Transform in step 140. The marginal spectrum is the Hilbert Spectrum integrated through all time. In this simplification, the time coordinate is lost
25 as in the Fourier spectral analysis, which leaves a summary of the frequency content of the event. Therefore, this presentation should only be used when the phenomena being analyzed is stationary. Formally, the marginal spectrum $h(_)$ is defined as:

$$h(w) = \int_0^T H(w, t) dt \quad .16$$

Because there is no analytic expression for $H(_, t)$, the integration can only be performed in a computer as a sum.

An example of a marginal spectrum is shown in Figure 7.

More particularly, Figure 7 shows the corresponding marginal spectrum of the Hilbert Spectrum given in Figure 6(a).

The frequency in either $H(_, t)$ or $h(_)$ has a totally different meaning from results generated by applying Fourier spectral analysis. In the Fourier representation, the existence of energy at a frequency, $_$, means a component of a sine or a cosine wave persisted through the time span of the data.

In contrast, the existence of energy at the frequency, $_$, means only that, in the whole time span of the data, there is a higher likelihood for such a wave to have appeared locally. In fact, the Hilbert Spectrum is a weighted, non-normalized, joint amplitude-frequency-time distribution. The weight assigned to each time-frequency cell is the local amplitude. Consequently, the frequency in the marginal spectrum indicates only the likelihood of an oscillation with such a frequency exists. The exact occurrence time of that oscillation is given in the full Hilbert spectrum.

To illustrate this difference, the corresponding Fourier Spectrum of the wind speed signal is also given in Figure 7 using a dotted line. As can be observed, there is little similarity between the Fourier spectrum and the marginal spectrum. While the Fourier spectrum is dominated by the DC term because of the non-zero mean wind speed, the marginal spectrum gives a nearly continuous distribution of energy. The Fourier spectrum is meaningless physically, because the data is not stationary. In contrast, the marginal spectrum

provides a physically meaningful interpretation of the wind speed signal.

Instantaneous Frequency

5 There are two types of frequency modulation: the inter-wave and the intra-wave modulations. The first type is familiar because the frequency of the oscillation gradually changes as the waves disperse. Technically, in dispersive waves, the frequency is also changing within one wave, but
10 that is generally not emphasized either for convenience, or for lack of a more precise frequency definition. The second type is less familiar, but it is also a common phenomenon: if the frequency changes from time to time within a wave its profile can no longer be a simple sine or cosine function.
15 Therefore, any wave profile deformation from the simple sinusoidal form implies intra-wave frequency modulation.

 In the past, such phenomena were treated as harmonic distortions. Nevertheless, such deformations should be viewed as intra-wave frequency modulation because the intra-wave
20 frequency modulation is a more physically meaningful term.

 In order to understand these frequency modulations, the invention applies a unique definition of instantaneous frequency. This definition stems from the EMD method and requires the signal to be reduced into IMF components. After
25 extracting the IMF components, an instantaneous frequency value can be assigned to each IMF component. Consequently, for complicated data in which more than one IMF may be extracted by EMD, there can be more than one instantaneous frequency at a time
30 locally.

 With the Hilbert Transform, a unique definition of instantaneous frequency may be applied by the computer implemented method as illustrated by step 160. Step 160

calculates the instantaneous frequency which is formally defined as follows:

$$w(t) = \frac{dq(t)}{dt} .17$$

By calculating instantaneous frequency, step 160 of the invention permits the frequency value to be defined for every point with the value changing from point to point.

The validity and the implications of the instantaneous frequency for nonlinear signals may be analyzed by examining an idealized Stokes wave in deep water. The wave profile of such a Stokeian wave is modeled by

$$X(t) = \cos(wt + e \sin wt) \quad 18$$

Therefore, it is an intra-wave frequency modulated signal. Approximately, equation (18) can be shown to be:

$$X(t) = (1 + e) \cos wt + e \cos 2wt + \dots \quad 19$$

The wave profile is also shown in Figure 9(a). Because the intra-wave frequency can only be approximated by harmonics in Fourier analysis, we can still have the same profile, but not the same frequency content. The wave form shows sharpened crests and rounded off troughs, which make the crests and troughs asymmetric with respect to the mean surface.

Processed with computer implemented EMD, this data yields only one IMF component as shown in Figure 9(b), with a constant offset component (not shown). Although this wave has only one characteristic scale or IMF, the Wavelet analysis result shown in Figure 9(c). Figure 9(c) has many harmonics with two visible bands of energy corresponding to the highest order of approximations of the possible harmonics.

In contrast, the IMF data can be processed by the inventive method to give the Hilbert Spectrum shown in Figure 9(d). The Hilbert Spectrum has only one frequency band centered around 0.03 Hz, the fundamental frequency of the wave train, but there is an intra-wave frequency modulation with a magnitude range of 0.02 to 0.04 Hz as the model truly represents. This intra-wave frequency modulation has been totally ignored in the past, for the traditional definition of frequency is based on the reciprocal of periodicity and Fourier Analysis.

Instantaneous Energy Density

Furthermore, the computer implemented method may also calculate the instantaneous energy density in step 150. The instantaneous energy density, IE, is defined as:

$$IE(t) = \int_{\omega} H^2(\omega, t) d\omega \dots\dots\dots 20$$

Still further, this instantaneous energy density depends on time. Therefore, the IE can be used to check energy fluctuations.

Stationarity

To quantitatively measure the stationarity of a physical signal, the invention utilizes step 165 to calculate various stationarity measurements. Before introducing the preferred stationarity measurements, a brief review of conventional stationarity measurements is presented.

The classic definitions of stationarity are dichotomous: a process is either stationary or nonstationary. This crude definition is only qualitative in nature. Such definitions are both overly stringent and useless at the same time: few data sets can satisfy the rigor of these definitions; consequently, no one even bothers using them to check

stationarity of the signal. As a result, data as nonstationary as earthquake and seismological signals are routinely treated as stationary (see, for example, Hu, et al., 1996., *Earthquake Engineering*. Chapman & Hall, London).

Sometimes, for some obviously nonstationary data, two less stringent definitions are invoked: piece-wise stationary and asymptotically stationary. These definitions are still dichotomous.

To quantify the statistical processes further, an index is needed to give a quantitative measure of how far the process deviates from stationarity. A prerequisite for such a definition is a method to present the data in the frequency-time space.

With the energy-frequency-time distribution (Hilbert Spectrum) described above, stationarity of the physical signal may be quantitatively determined. Therefore, the invention introduces an index of stationarity as follows and calculates a Degree of Stationarity in step 165.

The first step in defining the Degree of Stationarity, **DS(_)**, is to find the mean marginal spectrum, **n(_)**, as

$$n(w) = \frac{1}{T} \int_0^T h(w) dt \dots\dots\dots 21$$

Then, the Degree of Stationarity may be defined as:

$$DS(w) = \frac{1}{T} \int_0^T \left(1 - \frac{H(w, t)}{n(w)} \right)^2 dt, \dots\dots\dots 22$$

Again, the value of DS(_) can be determined by the computer.

Therefore, the specialized computer 410 according to the invention can be treated as a stationarity meter.

For a stationary process, the Hilbert spectrum cannot be a function of time. Then, the Hilbert Spectrum will consist of

only horizontal contour lines and $DS(_)$ will then be identically zero. Only under this condition will the marginal spectrum be identical to the Fourier spectrum, then the Fourier spectrum will also make physical sense. On the other hand, if the Hilbert spectrum depends on time, the index will not be zero, then the Fourier spectrum will cease to make physical sense.

In general, the higher the index value, the more nonstationary is the process. The DS for the wind data is shown in Figure 8(a). As the index shows, the data are highly nonstationary especially for the high frequency components.

Eq. (22) defines the stationarity as a function of frequency. This is necessary because certain frequency components can be nonstationary while other components remain stationary. An example is sporadic riding wind-generated waves on otherwise uniform swell: the low frequency swell component is stationary, while the high frequency wind waves are intermittent, and hence nonstationary.

The degree of stationarity can also be a function of time implicitly, for the definition depends on the time length of integration in Eq. (22). Therefore, a process can be piecewise stationary. On the other hand, for a singular outburst in an otherwise stationary signal, the process can be regarded as almost stationary if a long time integral is performed, but nonstationary the integral only encompasses the immediate neighborhood of the outburst.

Stationarity can be a complicated property of the process: for any signal shorter than a typical long wave period, the process may look transient. Yet as the signal length gets longer, the process can have many longer wave periods and becomes stationary. On the other hand, the signal can be locally stationary while in a long time sense nonstationary. An index is therefore not only useful but also

necessary to quantify the process and give a measure of the stationarity.

The invention also calculates a Degree of Statistic Stationarity in step 165. The degree of stationarity defined in Eq. (22) can be modified slightly to include statistically stationary signals, for which the Degree of Statistic Stationarity, **DSS**(, **T**), is defined as

$$DS(w) = \frac{1}{T} \int_0^T \left(1 - \frac{H(w, t)}{n(w)} \right)^2 dt, \dots\dots\dots 23$$

where the over-line indicates averaging over a definite but shorter time span, **T**, than the overall time duration of the data, **T**. For periodic motions, the **T** can be the period. Such a time scale, however, is hard to define precisely for high dimensional, nonstationary dynamic systems.

Even with this difficulty, the definition for **DSS** could be more useful in characterizing random variables from natural phenomena. Furthermore, **DSS** will depend on both frequency and the averaging time span. For the wind data taken as an example, the **DSS** is given in Figure 8(a) with **T** = 10, 50, 100, and 300 time steps respectively. The results show that while the high frequency components are nonstationary, they can still be statistically stationary. Two frequency bands at 7 and 17 Hz are highly nonstationary as the **DSS** averaged at 100 time steps shown in Figure 8(b). These components are intermittent as can be seen in the IMF components and the marginal spectrum. A section of the original wind data is also plotted in Figure 8(c) to demonstrate that there are indeed prominent 7 and 17 Hz time scale oscillations.

Display of Selected Results

The invention displays various results of the above-described computer implemented method in step 190. These

displays are extremely useful in analyzing the underlying physics of the physical phenomenon being studied as described above. Furthermore, particular examples of these displays and the increased understanding of the underlying physics which these displays permit are discussed in the following section.

For example, the invention generates various Hilbert spectra displays in the display step 190. As mentioned above, both color coded maps and contour maps may be employed to display the Hilbert spectra in display step 190. In addition, the color coded maps convey information to the operator in a uniquely accessible way permitting a more thorough and deeper understanding of the physical phenomenon and may be considered as necessary to analyze some physical phenomena.

The displays generated by the invention in display step 190 are central to the invention because they allow an operator to analyze the underlying physics of the physical phenomenon being studied.

The display step 190 outputs displays to display 450. As mentioned above, display 450 includes devices such as a cathode ray tube and a flat panel display. As an alternative, display step 290 may generate a hard copy output by utilizing printer 460 or may send the generated display to output device 470.

BIOLOGICAL SIGNAL PROCESSING

The above description provides a foundation of signal analysis methodologies which has broad applicability to a wide variety of signal types. Once such applicable signal type is biological signals which are signals measured or otherwise representative of a particular biological phenomenon.

For example, any given physiological process has a number of quantities that can be measured to produce a signal or otherwise be represented by a signal. The invention can be applied to such signals in an effort to better understand the

underlying biological phenomenon. For example, the relationships between different biological variables can be studied with a precision and depth of understanding not possible before.

5 The invention can also be used to arrive at an analytical function representative of the biological phenomenon. By using the inventive filtering methods, the biological signal can be simplified to eliminate components not particularly relevant to the analysis and to thereby make it possible to
10 represent the signal with a function.

Blood pressure data, such as the data shown in Figures 9(a)-(g), are examples of the invention's applicability to analyzing and characterizing biological signals. This blood pressure data and the analysis that follows focusses on
15 changes in blood pressure over the course of day.

To collect this data, a pressure probe was implanted into the pulmonary artery of a rat. Measurements were taken with the rat under controlled conditions (e.g. rat breathing normal atmosphere at sea level, quiet room, lit for 12 of the 24 hour
20 time span, etc.). In the experiment, a Statham P23ID transducer was utilized, data collected by the computer 400, and also recorded on a chart recorder. A standard A/D converter was utilized to converted the transduced analog signal to digital data for storage and processing by the
25 computer 400. It is to be understood that this particular set-up is exemplary in nature and illustrates one of the various ways in which the biological data can be obtained for processing by the invention.

Figure 9(a) shows the results of measuring the rat's
30 blood pressure for a 24-hour period with the pressure waveform being sampled at a rate of 100 points/second. A one hour strip of this data is shown in Figure 9(b). Two separate 10-second strips of this data are shown in Figures 9(c)-(d) with 9(c) exhibiting less regularity than 9(d). Figures 9(e)-(f)

are the systolic peaks and diastolic troughs for the one hour record shown in Figure 9(b), obtained by connecting the successive peaks and successive valleys, respectively.

In order to compare the invention against conventional methodologies, Figure 10(a) is presented which shows the conventional Fourier Spectrum for the one-hour data of Figure 9(b). Figure 10(a) shows this Fourier Spectrum from which one can easily identify spectral peaks at 1.5, 6.5 and 13 Hz. The 6.5 Hz peak represents the heartbeats which necessarily affect blood pressure. The 13 Hz peak is the harmonic of the 6.5 Hz heartbeat peak. The 1.5 Hz peak is probably related to respiration.

Figures 10(b)-(c) show conventional Fourier spectra for the two 10-second sections of data (Figures 9(c)-(d)). Fourier analysis for the one-hour data of Figure 9(b) is shown in Figure 10(d) in which the locations of the highest peaks of the Fourier spectra in every 1-minute window are plotted on the time-frequency plane. A perspective view of the windowed 1-hour and 10-sec Fourier results are given in Figures 10(e) and 10(f), respectively and show the variation of the amplitudes of the signals.

Figure 10(g) directly compares the inventive results against conventional techniques. In Figure 10(g), the Fourier (dotted line) spectra and the Marginal Hilbert (solid line) spectra of the blood pressure data from Figure 9(c) are plotted together. As can be seen from this comparison, the Fourier spectra devotes a great deal of energy to the higher-harmonic components.

As explained above, the invention adopts the spacing of extrema values to analyze the data. Specifically, the sifting process is applied to the data to extract a set of intrinsic mode functions.

Figures 11(a)-(h) show the results of applying the empirical mode decomposition method of the invention to the

blood pressure data of Figure 9(c). As shown therein, the invention produces eight IMFs from this blood pressure data. The residual IMF R_8 is constant.

Figures 12(a)-(h) show the results of applying the Empirical Mode Decomposition method of the invention to the blood pressure data of Figure 9(d). As shown therein, the invention produces eight IMFs (C_1 - C_8) from this blood pressure data. The residual IMF C_8 (a.k.a R_8) is constant.

In Figures 12(a)-(h), the IMF components have very different amplitudes. The IMFs having the most energy are C_2 , C_3 and C_4 . The amplitude and periodicity of these three main components closely approximate their respective, constant levels.

By recognizing the main or most significant IMFs, one can reconstruct a filtered version of the signal that eliminates undesired components while continuing to faithfully represent the original signal. For example, Figure 13(b) shows a combination of IMFs C_2 , C_3 and C_4 . The sum of these components faithfully represents the original signal as can be seen by comparing the IMF sum in Figure 13(b) with the original signal in Figure 9(c).

Of course, other filters can be constructed with the IMFs. One such example is Figure 13(a) which shows a summation of IMFs C_1 , C_2 and C_3 that were calculated from the blood pressure signal of Figure 9(c).

Another filtering example is shown in Figure 13(c) which is a sum of IMFs C_4 , C_5 , C_6 , C_7 and C_8 shown in solid line. These components are the lower-frequency components and their sum recovers the slow variation of the pressure signal. The dotted line in Figure 13(c) shows the original pressure signal.

Figure 14(a)-(b) show the Hilbert spectrums of the IMF components derived from the Figure 9(d) and 9(c) blood pressure signals, respectively. Specifically, The Hilbert

spectrum of Figure 14(a) shows that the most prominent energy bands are centered at 6.5, 3.0 and 1.5 Hz. As shown, there are intra-wave frequency modulations in this spectrum which are indications of nonlinear dynamics. The wide fluctuations of frequency values in the Figure 14(b) Hilbert spectrum make
5 of frequency values in the Figure 14(b) Hilbert spectrum make any visual mean estimation exceedingly difficult.

By further applying the inventive methodologies, a marginal Hilbert Spectrum can be calculated by integrating the Hilbert Spectrum. An example is shown in Figure 10(g) which
10 uses a solid line to plot the marginal Hilbert spectrum of the Figure 9(c) blood pressure signal. Prominent spectral peaks occur at 7 and 1.3Hz.

Figure 10(g) also uses a dotted line to plot the corresponding Fourier Spectrum. By comparing these spectra, one can see that the mean peaks line up. However, the Hilbert spectrum clearly depicts the fluctuation of energy over frequencies without allowing the frequency of oscillation to be variable in the whole time window.

One basic difference between the conventional spectra of Figure 10(d) and the inventively derived spectra of Figure 14(a) lies in the stationarity hypothesis. In Figure 10(d), the Fourier spectrum assumes stationary oscillation. In Figure 14(a), the Hilbert spectra, does not make this assumption and is valid for nonstationary oscillations.
20

By using the invention, one can more readily and accurately recognize the various features of blood pressure signals. Moreover, the invention offers a more comprehensive view of the blood pressure fluctuation than the classical Fourier analysis.
25

The invention may also be used to study the effect of one variable on another variable. Specifically, by changing one variable of a system, measuring the effect on another variable, and then applying the invention one can arrive at a much deeper understanding of underlying system. The invention
30

also permits the modelling or representation of data with an analytic function that was not possible with conventional techniques.

5 Biological systems are examples of systems which can be better understood and modelled by applying the invention. Biological systems are often studied by changing one variable and recording the changes of other variables. The resulting data is often oscillatory, stochastic and non-stationary. Data having these properties are particularly susceptible to
10 processing by the invention.

A particular example elaborated upon here is the effect of changing the breathing gas concentration of oxygen on the blood pressure of an animal. Analyzing such stochastic data to obtain crystal clear results describing the effects of oxygen concentration changes on blood pressure has been impossible with conventional techniques such as Fourier analysis.

Concrete data illustrating this example is shown in Figures 15(a)-(d). Specifically, the pulmonary blood pressure in the arterial trunk of two rats breathing normal air at sea level is shown in the upper trace of Figures 15(a)-(b) with the lower trace showing the oxygen concentration.

These same rats were then subjected to step changes in oxygen concentration: Figure 15(c) shows a step increase and 15(d) shows a step decrease in oxygen concentration and the effect thereof on blood pressure. From this raw data, one can see certain trends. However, there is no definitive way to handle this overwhelmingly complex data to reveal the underlying physiological variations. Fourier analysis simply
25 does not work for such nonstationary signals. By applying the invention, however, which works particularly well with nonstationary signals, one can arrive at a much deeper understanding of the underlying physiology.

As described above in detail, the invention applies a unique Sifting Process. Figures 15(e)-(h) illustrate this Sifting Process as it is applied to the blood pressure signal of Figure 15(b). Specifically, Figure 15(e) illustrates generating the envelopes (dot-dash line) by connecting successive extremas (peaks and troughs) of the signal (solid line) with cubic splines. The mean of these two envelopes is shown in Figure 15(e) with a thick solid line and is denoted by the symbol $m_1(t)$.

The difference, $X(t)-m_1(t)$ is designated $h_1(t)$ as is shown in Figure 15(f). From this figure, it can be seen that $h_1(t)$ has a few negative local maxima and positive local minima, suggesting that further Sifting needs to be performed before the first intrinsic mode is generated by the invention and that the quantity $h_1(t)$ is not yet a true representation of an "oscillation about the mean."

To improve this situation, two definitive requirements are imposed for a function that represents the "oscillations about the mean": (i) in the whole data set, the number of extrema and the number of zero-crossings must either be equal or differ at most by one, and (ii) at any time, the mean value of the envelope of the local maxima and the envelope of the local minima must be zero. An oscillatory function that is processed to satisfy these definitions is called an intrinsic mode function (IMF) as more fully described above.

The function $h_1(t)$ shown in Figure 15(f) does not satisfy this definition or the requirements of an IMF. Thus, further Sifting is performed by treating $h_1(t)$ as the new data set and repeating the Sifting Process including determining the new upper and lower envelopes, computing their new mean $m_{11}(t)$.

The difference $h_1(t)-m_{11}(t)$ is designated $h_{11}(t)$ which is treated as the new data set. The process is repeated a number of times (Figs. 16(g)-(h)) until it converges. The convergent

result, Figure 16(g), is designated by $C_1(t)$ and is the first intrinsic mode function, which has a zero local mean.

The difference between $X(t)$ and $C_1(t)$ is a function of time representing a "mean trend" after the first round of Sifting. It is designated as the "first residue" $R_1(t)$: $X(t) - C_1(t) = R_1(t)$

The first residue, $R_1(t)$, is again oscillatory and can be analyzed as new data by another round of Sifting in the Empirical Mode Decomposition Process, yielding the second intrinsic mode function $C_2(t)$ and the second residue $R_2(t)$. The process is continued until either the residue of the intrinsic mode function becomes less than a predetermined small number or the residue becomes nonoscillatory. The resulting IMFs are shown in Figures 16(a)-(p).

If the process takes n steps, the original signal $X(t)$ can be represented as follows:

$$X(t) = C_1(t) + C_2(t) + \dots + C_n(t) \quad 24$$

The last term $C_n(t)$ represents the nonoscillatory mean trend of the signal. As such, important information exists in this mean trend particularly for certain types of data.

The other terms C_{n-1} , C_{n-2} , etc represent the oscillatory portion of the mean trend. Each term represents a different spectral portion of the mean trend.

With the IMFs in hand, further processing is possible. One such processing technique is filtering in which certain IMFs are combined or summed while leaving out other IMFs.

For example, a low-pass filter or low-frequency representation $M_k(t)$ of the mean trend of the signal $X(t)$ can be generated as follows:

$$M_k(t) = C_k + C_{k+1} + \dots + C_n \quad 25$$

where $2 < k < n$

The lower the value of k , the more oscillations $M_k(t)$ contains. By adjusting the values of k and n , a variety of filters may be constructed each having desired characteristic(s).

Representing the original data, e.g. of Figure 15(a), with an analytic expression is not always possible or practicable. The invention, however, offers a technique of accurately representing the physically meaningful portions of a signal with an analytic function.

For example, when one examines the indicial functions that represent the changes of the signal $X(t)$ in response to step changes in oxygen concentration, one looks for changes in the mean trends $M_n(t)$, $M_{n-1}(t)$, and ... with respect to changes in O_2 level. To do this, it is helpful to fit the experimental result on $M_k(t)$ with an analytic function. Particularly, if one takes the origin of time $t=0$ at the time of imposing a step change in oxygen concentration, the resulting change in the mean blood pressure in response thereto for $t>0$ can be represented as:

$$M_k(t) = A_1 + A_2 e^{-l_2 t} + A_3 t e^{-l_3 t} + A_m t e^{-l_m t} \quad 26$$

where constants A_1, \dots, A_m and l_2, \dots, l_m may be determined with a conventional least-squares estimation technique.

The above estimation is greatly affected by the choices of k and m . By appropriately selecting k and m , different degrees of detail can be presented.

In reality, one can only approximate a step function change of O_2 . The dropping step of Figure 15(d) and the rising step of Figure 15(c) cause different changes in blood

pressure. Hence, two different empirical functions are utilized. For the first case, the equation is:

$$M_k(t) = p_m(t_0) \left[1 + A_1(t-t_0)e^{-\frac{t-t_0}{T_1}} + A_2(t-t_0)e^{-\frac{t-t_0}{T_2}} + A_3[1 - e^{-\frac{t-t_0}{T_3}}] \right], \text{ for } t_0 \leq t \quad (27)$$

5

for $t_0 \leq t$, where t_0 is the instant of time when O_2 concentration drops suddenly, and $p_m(t_0)$ is the measured value of $M_k(t_0)$. For the second case the following equation appears good enough:

$$M_k(t) = p_m(t_1) [1 + A_4[e^{-1(t-t_1)} - 1]], \text{ for } t_1 \leq t, \quad (29)$$

15 where t_1 is the time when the O_2 concentration increases suddenly. The variables A_1 , A_2 , A_3 and A_4 are dimensionless.

Taking the analysis into the spectral domain, the invention offers further tools. As defined above, the Hilbert transform of $X(t)$ is $Y(t)$. Hilbert has shown that the complex variable $Z(t) = X(t) + iY(t)$ is an analytic function of t and
20 can be written in polar coordinates as $a(t)\exp\{i\phi(t)\}$, thus defining the amplitude $a(t)$ and phase angle $\phi(t)$.

As further defined above, an instantaneous frequency $\omega(t)$ can be calculated from the derivative of $\phi(t)$ with respect to
25 time. Knowing the amplitude $a(t)$ and frequency $\omega(t)$ as functions of time, one can plot contour maps as shown in Figure 23(a). The contour maps of the amplitude as functions

of frequency and time are called the Hilbert amplitude spectrum, $H(_,t)$.

The vanishing of the local means of the IMF's C_1, \dots, C_{n-1} is a very important result because the amplitude $a(t)$ and phase angle $_(t)$ of the Hilbert spectrum are sensitive to the local means.

Using the definition above $\{M_k(t) = C_k + C_{k+1} + \dots C_n$, where $2 < k < n\}$ to represent the mean trend, the invention further defines the corresponding sum as follows:

$$X_k(t) = C_1(t) + C_2(t) + \dots C_k(t) \quad 30$$

to represent the oscillations about the mean trend $M_{k+1}(t)$. The Hilbert amplitude spectrum of $X_k(t)$ may be designated as $H_k(_,t)$. The square of $H_k(_,t)$ represents an oscillatory energy density. Thus, the invention also defines the oscillatory energy about the mean, $E_k(t)$, by an integration over all frequencies as follows:

$$E_k(t) = \int_0^2 H_k(w, t) dw \quad 31$$

The variations of $E_k(t)$ and $M_k(t)$ with oxygen level $O_2(t)$ yield the desired summary of information about the transient response of $X(t)$ to $O_2(t)$.

The oscillatory energy about the mean $E_k(t)$ is quite similar to the instantaneous energy instantaneous energy density, IE, described above. The difference is that the $E_k(t)$ is calculated from a subset (k) of the IMFs while IE is calculated from the full set of IMFs. In other words, the oscillatory energy about the mean is derived from a filtered version of the original signal in which a subset (k) of the IMFs is utilized to construct the filtered signal. This contrasts with instantaneous energy density which is derived from the full set of IMFs.

The oscillatory energy about the mean $E_k(t)$ is another nonstationary stochastic variable that can be treated in the same manner as outlined above. Specifically, the progression from steps 350 to 370 to 120 in Figure 1(d) provide a process for applying EMD to $E_k(t)$ to generate another set of IMFs. The IMFs thus generated may be further processed according to the techniques disclosed herein. The process may be repeated as many times as desired as indicated by the loop in Figure 1(d).

From the IMF's shown in Figures 16(a)-(p), one can compute the mean trend functions M_k from equation 25 set forth above. The results are shown in Figures 17(a)-(f) which are the main results to be used for the indicial response determination.

The next step (360 Figure 1(d)) is to generate analytic functions or otherwise perform a curve fitting process. This is a chief advantage of the present invention because for many data sets, such as the blood pressure data in Figs. 15(a)-(d), deriving analytic functions is impossible. By applying the inventive methodologies, however, deriving such analytic functions is possible. Specifically, the mean trend data extracts relevant data and removes unnecessary or irrelevant data thereby producing a simplified data set for which it is possible to derive an analytic function. The degree of simplification and extraction can be controlled by properly selecting which IMF components are included in the mean trend data.

The analytic representation of the indicial response functions of Figures 17(a)-(f) by equations 26-28 was done with a least-squares error method. The results are shown in Figures 18(a)-(c) and 19(a)-(c). These are the primary results of interest for tissue engineering analysis and design.

Specifically, the results shown in Figures 18(a)-(c) and 19(a)-(c) provide indicial response functions of the mean

pulmonary blood pressure at the arterial trunk in response to a step decrease or a step increase in breathing gas oxygen concentration. A similar analysis can be directed toward the oscillation modes defined by equation 29.

5 The oscillation modes for $k=1, 2, 4$, and 6 are respectively shown in Figures 20(a)-(d). The signals shown in these figures contain a lot of information that needs to be extracted into simple, understandable terms. This can be done by applying the Hilbert transform and generating the Hilbert spectrum. The results are shown in Figures 21, 22(a)-(h), 10 23(a)-(b). Specifically, Figure 21 is a plot of the oscillatory energy defined by equation 29 as a function of time. This spectrum is analyzed as a nonstationary random signal by the invention to resolve it into oscillatory IMF modes and mean trend functions $M_k(t)$, with the associated analytic functional representation as illustrated in Figures 15 22(a)-(h) for $k=9, 10, \dots$, and 16 .

20 To further analyze the data, the results of calculating the instantaneous frequency and amplitude of oscillations of the pressure signal $X(t)$, made possible by the Hilbert transformation, can be plotted against time in a three-dimensional manner as shown in Figure 23(a). The same can be plotted two-dimensionally on the plane of time and frequency by the contour lines of equal amplitudes, as shown in Figure 25 23(b).

Figure 24 is a conventional FFT amplitude spectrum of the pressure signal in 1-min segments under the assumption that the process is stationary in each segment. This conventional spectrum provides a basis of comparison against the Hilbert spectra generated by the invention.

30 As mentioned above, Fourier analysis is based on the hypothesis of segmental stationary random oscillation, the principle of linear superposition of sine waves, and a global average of waveform convolution over each time segment. The

HHT is based on the hypothesis of nonstationary processes, the principle of linear superposition of nonlinear IMF's, and local determinations of amplitude and frequency (through differentiation rather than convolution) of each IMF. In terms of the IMF, the first k modes can be added together the represent oscillations about the mean trend $M_{k+1}(t)$.

The Fourier series cannot represent time variation of a nonstationary signal and does not have a property or capability to separate a signal into two parts, one part representing a mean trend while the other part represents oscillations about the mean. The number of intrinsic modes, n, is finite: in general, $n < \log_2 N$, where N is the total number of data points. The number of harmonics in Fourier analysis is N/2.

Comparison of the Hilbert and Fourier spectra respectively shown in Figures 23(b) and 24 shows that both spectra display a major frequency component at approximate 5Hz where the energy is concentrated. This is close to the heart rate of the rat subject. This rate decreases when the oxygen concentration is decreased. These two spectra are in different vertical scales. The Hilbert spectrum contains no energy with frequency > 10Hz, and it also has fewer yet more diffused frequency bands than the Fourier spectrum. This is because the Hilbert spectrum gives only the global mean. The mean values certainly will show less variations.

The Fourier spectrum of Figure 24 contains more frequency bands because any deviation of the waveform from the basic sinusoidal harmonic will result in strong higher harmonics whereas the Hilbert spectrum allows variation of instantaneous frequencies, hence the fuzzy spread in the frequencies. This calls attention to the fact that the heart rate is also a stochastic variable, which could be studied by the inventive methods disclosed herein. The strong higher harmonic band

with frequency > 10Hz in the Fourier spectrum is probably spurious. In other words, the Fourier components above 10Hz (starting at around 15Hz at time 0) have no physical meaning.

In contrast, the inventive results of Fig. 23(b) show a rich variety of low frequency components thereby conveying important information not available in the conventional result of Fig. 24. Thus, the invention is capable of more a more accurate physical representation of the underlying phenomenon than conventional Fourier-based analysis. Moreover, the clarity of the set of mean trends and the corresponding set of the oscillations is a unique contribution of the invention.

Thus, the invention provides useful tools for concisely and precisely describing the affect of changing one variable on another variable. The effect on blood pressure caused by changing the O₂ concentration provides a good illustrative example of these tools.

To further illustrate the broad applicability of the invention and its potential as a diagnostic tool, an abnormal condition (disease) was chosen. The particular abnormal condition chosen for illustration purposes is sleep apnea. This is a common condition in which the airway is temporarily obstructed during sleep causing the subject to eventually gasp for air. To study this condition, heart rate data was taken from a subject as shown in Figure 25. More accurately, the data is a measure of the time interval between pulses (pulse interval) of the heart plotted against time. Thus, small values indicate a fast heart rate and large values indicate a slow heart rate. This data includes a normal data section and an abnormal data section, both of which are labelled.

As will be shown in detail below, the invention provides powerful tools for studying this condition. Although the results to date are preliminary, they do indicate that the invention is capable of diagnosing this condition. Of course,

further studies are necessary before a reliable diagnosis can be made using the invention.

To improve the analysis, the data of Figure 25 was processed to make the spacing between data points even.

5 Furthermore, a section of the normal data (no apnea episode) was extracted for separate analysis. A blowup of the normal data having even spacing between data points is shown in Figure 26. A further blowup is shown in Figure 28.

10 The data of Figure 26 was then subjected to the inventive EMD to produce eight IMFs, C_1 - C_8 , as shown in Figures 27(a)-(h). The resulting IMFs provide important, and heretofore unavailable, data to a person attempting to gain a better understanding of sleep apnea particularly when these normal IMFs are compared against abnormal (apnea) IMFs.

The IMFs of Figures 27(a)-(h) were then utilized to construct the Hilbert Spectrum shown in Figure 29. This Hilbert Spectrum provides additional information about normal sleep patterns and how they are reflected in the subject's heart rate.

20 To continue the analysis, an abnormal data section (Figure 30) was subjected to the inventive EMD to produce eight IMFs, C_1 - C_8 , as shown in Figures 31(a)-(h). The third IMF C_3 is believed to be particularly important in analyzing and perhaps even diagnosing sleep apnea.

25 Figure 32 is a blowup of the abnormal data of Figure 30. The abnormality is apparent around second 5005 where the airway is temporarily blocked thereby causing the heart to race in an effort to extract the diminishing oxygen still available in the lungs. The sharp spike just after second
30 5005 illustrates the gasping breath and the resulting sharp increase in the pulse rate interval (corresponding to a decrease in the heart rate).

Figure 33 is the resulting Hilbert Spectrum of the abnormal data of Figure 30. Comparisons between the normal

Hilbert Spectrum of Figure 39 with the abnormal Hilbert Spectrum of Figure 30 yields further information for studying and understanding sleep apnea.

To further illustrate the wide applicability of the invention, it was applied to study epilepsy. Epileptic seizures occur when the brain's neurons fire in synchronism. The sequence starts from an epicenter and then propagates to an entire hemisphere of the brain. Even at this stage, the patient can still function in a relatively normal manner. When the synchronization propagates to both hemispheres of the brain, then the patient will suffer a seizure.

To study epilepsy, heart beat rate data was chosen. Figure 34 shows heart rate data (beats per minute) that was collected from a patient before, during and after a seizure. The time 0 is the starting point of the seizure.

Figures 35(a)-(i) show the IMF generated by the inventive EMD method applied to the Figure 34 data. These IMFs reveal important and physiologically meaningful data not available to a researcher before the application of the present invention.

Figures 36(a) and (c) illustrate two IMFs (modes 1 and 3) which may be utilized to correlate the data and study epilepsy. These IMFs are shown in alignment with the original heart rate data (Figure 36(b)). As is apparent from these figures, the first and third have components that appear to correlate with the onset of a seizure.

The Hilbert Spectrum of Figure 37 was generated by the invention from the data of Figure 34. The trace along 18 to 20 cycles/min correlates to time 0, the start of the seizure. To compare the invention against conventional techniques, a corresponding Wavelet Spectrum is shown in Figure 38.

As can be seen by the above illustrative examples, the invention is a powerful tool capable of analyzing data and producing new, quantitative measurements that enhance the understanding of the underlying phenomenon producing the data.

The IMFs themselves are important results of the inventive data analysis techniques and permit one to gain a level of understanding not possible with conventional techniques.

Although blood pressure, heart pulse interval, and heart rate data provide good examples of the invention's applicability to biological signals, it is to be understood that a large variety of other biological signals may be processed by the invention to gain a better understanding of the underlying biological process(es). Other examples include plethysmogram signals, electro-encephalogram (EEG) signals and temperature signals. Furthermore, the signal need not be taken from a living body and include in vitro studies such as current flow across membranes (patch clamping), fluorescence in confocal microscopy, spectroscopic signals, etc.

As mentioned above, the invention is also not limited to biological signal processing and includes the full range of real-world, data representative of an electrical, chemical, mechanical, optical, geophysical processes or phenomenon or combinations thereof all of which fall under the term "physical signal" as it was defined in the parent application.

Even further, the invention provides tools for studying the influence of one variable on another variable in a multi-variable system. The effect of hypoxia on blood pressure provides one illustrative example of this analysis. However, it is to be understood that any physical signal in a process or phenomenon having multiple variables of which the physical signal is one can be analyzed with the invention.

ALTERNATIVE EMBODIMENTS OF BIOLOGICAL SIGNAL ANALYSIS

As described above, the invention constructs upper and lower envelopes 20, 30 with a cubic spline in steps 210 and 230, respectively and in step 560. This cubic spline fitting, however, has both overshoot and undershoot problems. These problems can be alleviated by using more sophisticated spline

methods, such as the taut spline in which the tension of the spline curve can be adjusted.

Another alternative is higher-order spline fitting. Although such higher-order spline fitting may be more accurate, it will, however, introduce more inflection points or extrema, and consume more computing time. Therefore, it is not recommended as a standard operation. Only in special cases, it may be tried.

As the spline fitting procedure is time consuming, more efficient methods can be devised by using simple mean values of successive extrema instead of computing the envelope-mean. In this way, only one spline fitting is required rather than two. Although this alternative is easier and faster to implement, the shortcomings are more severe amplitude averaging effects when the neighboring extrema are of different magnitudes. The successive-mean method will have a stronger forcing to reach uniform amplitudes, in which the true physics associated with amplitude will be destroyed. Therefore, the successive-mean method should only be applied where the amplitudes of the physical signal components are constants.

Either the envelope mean or the successive mean method, when applied with the requirement of absolute symmetry, will produce the absurd result of uniform amplitude IMF's.

Therefore, the criteria in the Sifting Process should be chosen judiciously. One should avoid too stringent a criterion that we would get uniform amplitude IMF's. On the other hand, one should also avoid too loose a criterion that would produce components deviating too much from IMF's.

It is well known that the most serious problem of spline fitting is at the ends, where cubic splines can have wide swings if left unattended. As an alternative, the invention may utilize a method of adding characteristic waves at the

ends of the data span. This confines the large swings successfully.

The method of adding characteristic waves is not conventional. In contrast, the conventional window that is often applied to Fourier transform data results in loss of useful data. To avoid this data loss and to confine swings at the ends of the data span, the invention extends the data beyond the actual data span by adding three additional characteristic waves at each end of the data span.

The characteristic waves are defined by the last wave within the data span at the end of the data span. In other words, a characteristic wave is added to each end of the data span having an amplitude and period matching the last wave within the data span. This characteristic wave is a sinusoidal waveform that is extended three sinusoidal wave periods beyond the data span at each end. This process is repeated at the other end of the data span. In this way, spline fitting at the end of the data span, which can otherwise have a wide swing, is confined. In other words, by adding the extra characteristic waves at the ends beyond the data span, the spline curve will be tied down so that it will not have wild or excessive swings that would otherwise corrupt the data processing and analysis that utilizes these cubic splines.

Other than the spline fitting, the Hilbert transform may also have end effects. Because the first and the last points of the data are usually of different values, the Fourier transform will introduce additional components to bridge over the difference resulting in the well-known Gibbs phenomena. To eliminate it in the Fourier transform, various windows have been adopted (see, for example, Brigham, 1974, "The fast Fourier Transform", Prentice-Hall, Englewood Cliffs, NJ).

Instead of a window which will eliminate some useful data at the end, the invention again adds two characteristic waves

at either end. These waves all start from zero at the beginning, and end at zero at the end. Thus, the annoying Gibbs phenomena are greatly reduced.

Still further, the Hilbert transform needs over-sampled data to define the instantaneous frequency precisely. In Fourier analysis, the Nyquist frequency is defined by two points per wave, but the frequency is defined for a wave covering the whole data span. In the invention, the instantaneous frequency is defined through a differentiation process, and thus more data points will help defining the frequency more accurately. Based on the inventor's experience, a minimum number of data points to define a frequency is five (or four Δt 's). The lack of fine time steps can be alleviated through interpolating more points between available data. As a spline interpretation would also not create nor annihilate scales, it can also be used for the interpolation when the data is very jagged from under-sampled data. The smoothed data though have a longer length and are sometimes easier to process. The interpolation may give better frequency definition.

ACOUSTICAL SIGNAL ANALYSIS

Referring to Figure 39, an application of the invention will be to analyze the acoustical signal through the Hilbert-Huang Transformation (HHT), which consists of the Empirical Decomposition Method (EMD) and the Hilbert Spectral Analysis (HSA). Essentially, the signal will be decomposed into the Intrinsic Mode Function Components (IMFs). This decomposition is outlined in Huang's publications and patents. Once the invention decomposes the acoustic signal into its constituting components, all the operations can be performed on these components.

Speech analysis and speaker identification:

Referring to Figures 41 and 42, we will first discuss the way HHT analyzes speech. Then, based on the analysis results, we can discuss how to identify a speaker, i. e., to single out one speaker from others. Let us start with the following example.

Two speakers both said 'Halloo,' and the acoustic signals are digitalized at 44100 Hz with 16 bits resolution as shown in Figure 45a for a male speaker, and b for a female speaker. The EMD decomposed IMF components are given in Figure 46a and b. Each signal consists of 12 components, and each component consists of 30,000 points. They are plotted with the same vertical scale in Figure 46. As the IMFs are the results of scale separation of the original signals, each component represents different time scales, which can be translated to the frequency ranges. It should be pointed out that this frequency separation is not in the Fourier sense, for the signals separated in scale could be nonlinear; therefore, it can contain both sub and super harmonic components in Fourier frequency space. Consequently, the decomposition is not necessarily narrow banded in Fourier sense, but, as explained in Huang (1999), this decomposition preserves all the nonlinear properties of the signal. One can immediately see from these figures that the two decompositions contain very different IMFs. For the signal given in Figure 45a, the decomposition is given in Figure 46a. There, we have very regularly periodic signals for all the IMFs. Comparing this with the corresponding results in Figure 46b from the second speaker, we can see the differences. The second speaker does not have the regularity in the time scale. In the second speaker's results, we can see that the strongest signal is the third component, but for the first speaker the corresponding component is relatively weak. By the time we come to the 6th component of the first speaker, the component is still very strong, but there is almost no more signal in the second

speaker's result in Figure 46b. The richness of the low frequency components for the male speaker, and high frequency for the female speaker should be expected. This difference in frequency components can be seen vividly in the Hilbert spectral analysis as follows.

From these components, we can construct the Hilbert Spectra as given in Figures 47a and b, in which time-frequency-energy representation of the signals are presented, with the corresponding narrow banded Fourier based spectrograms given in Figures 48a and b constructed with 1028 sampling points in the window, which corresponding to the window width of 43Hz. In these figure, the total frequency range is represented by 200 bins to cover the frequency range from 0 to 10,000 Hz. In Figure 47a, we can identify a clear consistent low frequency energy concentration near 100 to 200 Hz, but there is no equivalent energy at this low a frequency in Figure 47b. To examine the results in more details, we have given the Hilbert spectra of the cases presented in Figure 47a and b in Figures 49a and b, in which the same 200 frequency bins are reassigned to cover the frequency range from 0 to 1,000 Hz. In these new and more detailed presentations of the signals, we can see that the male voice represented by the Hilbert spectrum by Figure 49a contains a strong modulated energy below or around 100 Hz, while the female voice represented by the Hilbert Spectrum given in Figure 49b contains the most energetic modulated components above 100 Hz. Furthermore, the female voice also contains wider range of high frequency energy distributions. In Figure 49, we can see the regular spaced vertical striations in the Hilbert spectra, which are the indications of the resonant beat period from the speaker's vocal cavities. This beat pattern can be easily seen from the IMF components, which can serve as crucial data for speaker identification too.

In order to show the unique properties of the HHT analysis results, we decided to examine the male voice in more details as follows: First, we give the spectrum it wide banded Fourier spectrogram as in Figure 50, constructed from 128 sampled points in a window, which corresponds to a wide banded spectrogram with band width of 344.5 Hz. Clearly neither the narrow nor the wide banded spectrograms give us any detailed information. This is shown even more clearly if we present the detailed views in Figure 51a and b, in which the spectrograms are plotted for the frequency range between 0 to 1000 Hz, corresponding to the condition represented in Figure 49a. The comparison is clear, while the Fourier based spectrograms could give us some qualitative information, the results is so crude that they cannot be used as a based for any serious acoustic signal analysis.

In order to emphasize the superior performance of the HHT, we also process the same data with Morlet Wavelet analysis, a continuous Wavelet analysis. The result is given in Figure 52a and b. These figures clearly identify the different time-energy-frequency distribution characteristics between male and female speakers, the strong high frequency energy concentration for female and the strong low frequency energy concentration for the male speaker. This clear difference aside, the Wavelet results really lacks the detailed analysis ability of HHT. When on comparing the pair of Figures 52a and b with those in Figures 49a and b, one can immediately see the lack of time-frequency resolution of the Wavelet results. These differences have been discussed in great details by Huang et al (1998, 1999).

To illustrate the lack of resolution in the Wavelet analysis further, we can smooth the Hilbert Spectrum result given in Figure 49a by filters in 100 and 200 time-steps. The results are given in Figures 9a and b respectively. By the time we smoothed the results with filter width of 200 points,

the results are clearly much smoother, but we will never
obtained the kind of overly smoothed result given by the
Wavelet, for the two analysis methods are very different: The
Hilbert spectrum gives the genuine instantaneous frequency
5 based on an adaptive basis totally independent of the kind of
a *priori* basis adopted in the Wavelet analysis. Furthermore,
the components in HHT are almost orthogonal, which gives no
energy leakage among different modes. The continuous Wavelet,
on the other hand, has a non-orthogonal representation. The
10 energy leakage among different frequency bands, and the over
redundancy have rendered the method to only extract
qualitative information.

The detailed time-frequency-energy presentation gives us
many more reference points for speaker identification and
verification. The continuous modulation of frequency and
energy will provide more reference points to separate one
speaker from the other. HHT analysis could also identify
peculiarities of one speaker from another. All these details
just cannot be found in any other analysis method.

20 To summarize the material discussed in this section, we
will first give a flow chat of speech analysis: Speech
containing various phonemes will be recorded, and the signal
will pass through the sifting process to get the IMFs. In
this step, the critical task is to identify the phonemes and
25 formants (Hilbert Spectra) for each sound element with
modulations in both frequency and amplitude as functions of
time. Databases will be build from the recorded speech data.
Such analysis is not available from any other method of
analysis.

30 There are two types of speaker identifications: to
verify that the speaker is a known person, and to separate the
speech from different speakers. The essential steps for both
tasks are as follows:

To verify a known speaker, we have to have the database of the targeted speaker built ahead of time. The database can be built following the steps listed in the speech analysis. To separate speakers from one another, we can record the speakers and analyze their speech as listed in the speech analysis part. Once the analyses are done, we can compare the details of the Hilbert spectra in their over all and the details of the spectral patterns, including the beat periods for the same phoneme and formant. Given the super temporal and frequency resolutions of the Hilbert spectra, the Hilbert spectra actually give a much better formant representation. With so many details in the Hilbert spectra, we can use many features as references. In the example given in this section, the overall pattern is sufficient.

For Speech recognition:

Speech analysis such as speech recognition as shown in Figure 42, the goal is not to identify a specific speaker. Rather the task is to identify the meaning of an utterance so that the commands contained in the speech can be translated into actions as in man-machine interaction. Because, the speakers can have a variety of accents, the approach is to obtain a limited number of uniquely identifying parameters to define the meaning of the utterance, rather than to obtain more and more detailed descriptions of the sound. In such applications, two approaches can be adopted for the HHT.

The first is by smoothing as in the cases of Figure 53a and b. More smoothing can be obtained by time-frequency averaging, rather than just time smoothing described here. The Laplacian filter is readily available. However, for most acoustic signal applications, there are lot more time steps than possible frequency bins. Therefore, time-wise smoothing is a more logical approach. Other than smoothing to obtain the time-frequency-energy pattern as means for recognition,

the formants identification is also a powerful method. Here we will discuss this approach as follows:

Formants by definition are the few characteristic time-frequency distribution of the maximum energy concentration in a speech section analyzed with filter bank or spectrogram methods (see, for example, Rabiner and Schafer, 1978). Conventionally, to make the number of components manageable, the formants are defined from the low frequency components only. The ideal of formant is to sharpen the poor time-frequency analysis in the spectrograms. Similar approaches have also been explored by Carmona et al (1997) using Wavelet analysis. As discussed by Huang et al (1998, 1999), the inherited poor time-frequency resolution cannot be overcome by post analysis smoothing or selection. The only alternative is to change to a genuine instantaneous frequency analysis as in the HHT, which in form and in substance is a much better formant representation of the speech. Let us examine an example. If we take the beginning of the sound for 'Halloo' signal, and analyze it with HHT, the result is given in Figures 54a and b. This is actually the consonant part of the 'h' sound. These figures, in fact, are simply obtained by the enlargement of the same section of the figure of 47a and 49a. One of the great advantages of HHT is that the frequency is defined by differentiation; therefore, we can breakthrough the limitation of the uncertainty principle and expanding the results to the limit of the sampling rate.

Figure 54a is the expansion of Figure 47a, while Figure 54b is the expansion of Figure 49a, both with the original signal plotted. Here we have the lower frequency emphasized. The continuous lines of the time-frequency curve are in form and substance a better formant. But they are indeed better defined than the conventional formants, for they also included the nonlinear deformation of the signal rather than assigning all the waveform deformation to harmonics. As the frequency

is defined by differentiation, the information provided here
is might be too much. If that is the case, the frequency
variation can be simplified by smoothing either through
filtering, or defined as differentiation with larger time
steps.

The essential steps for this task can be summarized in
the following flow chart: Again, we have to establish the
database consisting of templates of the key phonemes and
formants. In this case, the templates will be constructed
from the averaged value of a large number of different
speakers. In addition to the averaged value, the range of
scattering from the differences will also be recorded. When a
new speech is given, the record will be analyzed as in the
previous part to have the speech breakdown to phonemes and
formants. Each sound element will be compared with the
existing templates and identified. The identified sound will
be put together, and translated into sentences. Grammar check
and corrections should be made here to guarantee that the
speech makes sense. The final text will then be translated
into instruction for further actions, such as an order to a
servomechanism.

Speech synthesis:

Referring to Figure 40 the speech synthesis problem has
been review recently by Breen (1992). Basically, the
synthesis is based on a phoneme base. Having established the
analysis part, we can take sections of the sound record as
phonemes and build a database for it. This phoneme database
can then be used to synthesize speech. The advantage of this
phoneme base has the unique advantage over the conventional
one in that no local stationary assumption has been evoked.
Therefore, the frequency is continuously modulating, which can
make the final result sounds more naturally.

The detailed time-frequency-energy distribution results given by the HHT also give us a means to synthesize sound with higher fidelity, for the frequency modulation can be truly simulated by the instantaneous values in frequency and energy.

5 This overcomes one of the fundamental shortcomings of the Fourier based analysis, in which a local stationary assumption is to be invoked. This piecewise stationary analysis simply cannot closely simulate the constantly modulated frequency modulation as shown in the Hilbert spectral analysis results.

10 Also from Figures 54a and b, we can define the beginning of the speech clearly and un-ambiguously. The separation of syllables has also been a hard problem in speech analysis and synthesis.

A key to the potential value of our approach is that HHT gives time varying modulation of frequency and amplitude. The essential steps are as follows:

Based on the database of all the phonemes and formants, we can translate the given text to the time varying IMF components from the database. This translated data is checked again with prosody patterns, and synthesized into sound.

Speech quality enhancement:

Referring to Figure 43 one of the most important applications of acoustic signal analysis is to enhance the speech quality. For example, during the utterance of the word, 'Halloo,' a noise simulated by the drop of a spoon on the table was also heard. How to separate this noise from the speech signal is an important application. Traditionally, the cleaning up of a speech is carried through filtering. But Fourier based filtering has inherited shortcomings: Localized signal in time is broad in frequency; localized signal in frequency is broad in time. Furthermore, as discussed above, the generating mechanisms of most consonant sound are

nonlinear; therefore, most of the consonants, the information carrying sounds, have a lot of sub as well as super harmonics. We cannot remove certain frequency without altering the harmonics of other sound signal, which will down-grade the filtered result through loss of the harmonics. Here we propose the filtering through EMD. The filtering strictly by scale, the filtering here has to be implemented jointly in time-frequency space.

Let us examining the signal of the sound, 'Halloo + ding,' given as the top line in Figure 55. This signal is decomposed through EMD and we obtained the IMF components as given in Figure 56a and b. Figure 56a gives all the components with the uniform vertical scale, while Figure 56b gives the same information with the vertical scale in each IMF components normalized within its own frame. From Figure 56a, we can see that the 'ding' sound, occurring slight after 1.5 second mark, has the higher amplitude than any other IMF components. Figure 56b indicates that at the same time scale components with the 'ding' sound, there are also signals from the 'Halloo,' as indicated by the low level signal in c3. As a result, we cannot simply filter out the high frequency components by eliminating the first three IMFs.

Now we will accesses the performance of the EMD vs Fourier filtering. First, let us implement only the filtering by simply eliminate the first three IMF components. This approach is similar to the thinking of Fourier filtering as discussed by Huang (2000), but the result is not exactly the same. We will design this filtering as the "Fourier" type and discuss the difference later. The result certainly does not show the 'ding' sound any more. But this brute force filtering has also eliminated all the high frequency sound including some higher frequency elements from the 'Halloo' sound. The quality of the sound is degraded considerably. A better way is to eliminate the 'ding' sound in both time and

frequency space by selectively removing energy associated with the 'ding' sound. This was achieved by first studying each of the IMF component, identifying the 'ding' sections in each component by their sounds, frequencies, and occurrence time location. Then, selectively removing the sections that contain the 'ding' associated signals from each IMF component. After this is done, and separated 'Halloo' and 'ding' signals are represented by their respective IMF decompositions in Figures 57a and b. In Figure 57a, we can see that there is no longer signal associated with the 'ding' sound, while, in Figure 57b, we see the clear 'ding' sound stands by itself. The Hilbert spectra for the original and the EMD filtered signals are shown in Figure 58a and b. When all the IMF's are summed up, the re-constituted sound signals for 'Halloo' and 'ding' are given in Figure 55. The sound quality is so much improved over the brute force approach.

Next, we will implement the Fourier based filtering with two 48 degree FIR filters with cutoff frequency set at 2000 and 1000 Hz respectively. The filtered data with a cutoff frequency at 2000 Hz together with the HHT filtered data is given in Figure 59a. Based on the results plotted here, one can hardly see the difference. But if one pays attention to the relative darkness of the two side-by-side signals, one would see that Hilbert filtered signal is darker, an indication of more high frequency components being retained. Furthermore, if one plays the filtered data back through a speaker, we can immediately tell the difference, for there are still residual 'ding' sound in the Fourier filtered case. We then filtered the data with a similar filter but with a cutoff frequency set at 1000 Hz. This certainly eliminated the 'ding' sound, but the quality of the sound was very much downgraded.

The Fourier filtering is strictly in frequency space, while EMD filtering is in time scale. By operating in a rigid

frequency range, the Fourier filter will not eliminate the bounded super and sub harmonics of the signal outside of the pre-selected filtering frequency range. It, however, will remove the bounded super and sub harmonics of other signal components that happened to fall within this pre-selected frequency range, even if the fundamentals are outside this frequency range. As a result, through Fourier filter is localized in frequency, it actually affects signals of all frequency. In EMD, each IMF could be nonlinear; therefore, each of them is not banded limited in Fourier sense. By eliminating the first three IMF components, we still could have energy at Nyquist frequency in Fourier sense through the existence of the harmonics. So, through filtering by EMD, we can really limit the frequency to the components in time scale rather than in Fourier sense. This time space filtering will not influence the lower frequency components because it would leave the bounded super and sub harmonics of other components untouched, and it will also eliminate all the bounded super and sub harmonics associated with the selected time scale component. We have plotted the results of the Fourier spectra of the EMDT filtered, the "Fourier" type of filtering by eliminating the first three IMF components, the Fourier based FIR with cutoff frequency set at 2000 and 1000 Hz all in Figure 59b. As we discussed above, only by setting the cutoff frequency at 1000 Hz can we eliminate the 'ding' sound. The spectra showed the difference: Fourier filtering has eliminated all the energy at the high frequency range, but EMD filtering can leave some energy there. The result is a greatly improved voice quality.

Another application for the present invention is on music recording. Using EMD rather than Fourier based filter we can surgically remove the unwanted noises or sound to enhance the final quality of the product. As discussed above, the EMD filter is much more sophisticated than the Fourier based one,

for the EMD filter operates with the signal separated by temporal scales; therefore, it can keep track of the events precisely on the temporal axis. This operational principle is totally different from the Fourier based filter, which operates in Frequency space only. As discussed above, the localized signal in frequency space means the signal is uniformly distributed in time space, and localized signal in time space means uniform distribution in frequency space, it is just impossible to perform the precision surgical-like filter localized both in time and frequency spaces. Furthermore, many of the sound full of harmonics will be degraded no matter which frequency the Fourier filter will remove. In the EMD filter, however, the IMF components retained all the harmonics within a single scale component. The harmonics are represented by the frequency modulation as discussed by Huang et al (1998, 1999) and Huang (1999). Consequently, any filtering operation will not downgrade signal at other scales, which can still retain all its harmonics, if viewed in the Fourier sense.

A step in this task is to identify the unwanted sound in its time coordinate. It is impossible to blindly apply this method as in the traditional Fourier analysis to remove high frequency components. If that is the case, then we can also use EMD to remove the highest frequency IMF component. This approach has one unique advantage: By removing the highest frequency component locally or globally, it will not alter the quality of the low frequency sounds, for HHT does not depend on harmonics to represent nonlinear distortion of the waveforms of sounds. With the additional time tag, we can also implement HHT filter locally and globally with the precision unmatched by Fourier window-based filters.

If the unwanted sound is identified on the time axis, we can zero in the IMFs and test each component, or a combination of several components, to determine which one or which

components should be removed. Once the unwanted component (or components) is removed, the cleansed sound could be re-constituted locally.

5 **Acoustical signal storage and transmission:**

Acoustical signal storage and transmission might require limited bandwidth or data quantity. Using HHT, one could also reduce the amount of data to represent a given signal with acceptable, albeit reduced, quality. This can be achieved by re-sampling of the IMF components of longer time scales at a lower sampling rate. At the same time, we can also eliminate the short time scale components without too much of a reduction of the signal quality. The result of this re-sampling will enable us to store and transmit a given signal with reduced amount of data.

Data storage is a concern as the HHT is designed to examine the details of the signals. For storage, however, there are steps HHT can help. These steps are described as follows:

From the designed signals, decompose the data into IMFs. Test the recombined IMF without the highest few components to determine the degradation of the sound quality. Within the tolerable range, eliminate the maximum number of high frequency components. Re-sample the data by decimating (i. e., with large sampling steps). This will result in a smaller number of data, but also with slightly down graded sound quality.

Machine Operating Condition Monitoring

Referring to Figure 44 the acoustic signal emitted from an operating machine can be compared to a kind of speech made by the machine trying to inform us of its condition. A chipped gear, a broken bearing, a cracked shaft, a worn grinder, cutter, or saw blade will all send its distinct sound and

particular vibration signals. Such signals can be analyzed much the same way as speech signals discussed above. We will use a grinder as an example.

Figure 60a, b and c show the acoustical data from a grinder operating on a hard surface continuously for 95, 120, and 200 hours designed as TR095, TR120 and TR200 respectively. From the signals, it is hard to say whether the grinder operated at its optimal condition. Of course, the magnitude of the signal representing the loudness of the sound is increasing, but that alone is not a criterion for determining the condition of the grinder, for there might not be a *priori* record of the grinder at other time periods. Also from the record, we can determine the rotating speed of the grinder. The rotating speed is also changing. For the cases of TR120 and TR200, the rotating speed is 8,000 rpm; while the rotating speed for the case of TR095 is slightly higher at around 14,000 rpm. None of the above characteristics can be used as an indication of the health condition of the grinder.

To determine the health condition of the machine, one has to establish a criterion based on the condition of the machine at the time of monitoring. This can be implemented by HHT analysis. Using HHT analysis, we can first sift the data and obtain their IMF components as shown in Figure 61a, b and c. Then, we can also construct the Hilbert spectra from the IMFs as shown in Figures 62a, b and c. Here some distinct characteristics appear. When the grinder is sharp and operating smoothly, there is a clear frequency of the acoustic signature as in Figure 62a. The energy concentrates around the rotating speed as indicated. As the grinder becomes dull, it happens first to only part of the grinder surface. The noise generated by the dull part causes signal with greater amplitude or energy density. This intermittent acoustic signature occurs proportional to the dull surface of the grinder. This diffusion of acoustical signal can cover a much

broader range, but only intermittently. The intermittence, however, is only detectable by the HHT analysis as shown in Figure 62b. To the ear, the sound might still be continuous. As the wearing progresses, all parts of the grinder becomes
5 dull. At this stage, the acoustical signal will be a diffused signal everywhere as shown in Figure 62c.

The grinder is but only one example. Other telltale signs from the chipped gear, the broken bearing, the cracked shaft, the worn cutter, or saw blade can be identified in a
10 similar way.

To summarize the steps in machine health monitoring, we can state that this task is similar to speech identification. We can establish the templates database of normal and various abnormal operation conditions from the sound and/or the vibration signal of the machine. To diagnosis a machine, just record the operational sound and/or the vibration signal of the machine at any time to make comparison with the templates in the database to identify the problems. Knowing problems with existing templates, the problem can be identified. For safety sake, whenever the machine sound and/or its vibration signals are not within the tolerable range of the normal condition template, warning signal should be given.

The dependence on the existence of scale for mode
25 definition has a limitation in that the decomposition method cannot separate signals when their frequencies are too close. In this case, there would not be any characteristic scale: therefore, physically they are identical.

Particular Advantages of The Invention

The strength of the EMD method should be reiterated. EMD is built on the idea of identifying the various scales in the data which are quantities of great physical significance. Therefore, in the local extrema and curvature extrema Sifting

Processes, orthogonality is not a consideration, but scales are. Since orthogonal decomposition is a characteristic for linear systems, violating this restriction is not a shortcoming but a breakthrough. Therefore, the decomposed IMF's may or may not be orthogonal. As such, this method can be applied to nonlinear data. Though the IMF's in most cases are practically orthogonal, it is a coincidence rather than a requirement of the EMD.

Another advantage of the method is the effective use of all the data representing the physical phenomenon. In the Sifting Processes, the longest scale is defined by the full length of the data. As a result, EMD can define many long period oscillations. As is well known, the Hilbert transform without sifting tends to identify the highest frequency (Boashash, 1992, *"Estimating and Interpreting the Instantaneous Frequency of a Signal, Part I: Fundamentals"*, Proc. IEEE, 80, 520-538.), the extraction of the long period components is indeed a new feature of the EMD.

Finally, though the EMD method will give IMF components, the individual component does not guarantee well-defined physical meaning. This is true for all decompositions, especially for the methods with *a priori* basis. In most cases, however, the IMF's do carry physical significance. Great caution should be exercised in making such attempts. The rule for interpreting the physical significance of the IMF's is that the scales should be clearly separated. Together with the Hilbert spectrum, the totality of the presentation should give a much more detailed representation of the physical processes than conventional methods.

The invention being thus described, it will be obvious that the same may be varied in many ways. Such variations are not to be regarded as a departure from the spirit and scope of the invention, and all such modifications as would be obvious

to one skilled in the art are intended to be included within the scope of the following claims.